



Russian Federal Nuclear Center –  
Zababakhin Institute of Applied Physics



“ROSATOM” STATE CORPORATION

# Fluorescence molecular tomography using early arriving photons: fundamental equations, numerical experiment, and resolution analysis

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- 1. Introduction. What are the novelties?**
- 2. Basic expressions: fundamental equation and sensitivity functions**
- 3. Prototype of fluorescent tomograph and numerical experiment setup**
- 4. Reconstruction of fluorescence inclusions**
- 5. Spatial resolution analysis**
- 6. Conclusion and future research**



# Ways to improve the spatial resolution

- ❑ The development of models and methods for time-domain FMT with use of **early arriving diffuse photons**
- ❑ Application of **compressed sensing algorithms** to the reconstruction of fluorescence tomograms
- ❑ The development of methods for **mesoscopic FMT** and laminar optical tomography

# The novelties of our research

- We propose an original approach to macroscopic early-photon FMT based on a number of simplifications to derive the **analytic sensitivity functions** for reflectance geometry

V.V. Lyubimov, Opt. Spectrosc. 88: 282 (2000)

- To solve the FMT inverse problem we use an **original hybrid algorithm** that combines the algebraic reconstruction technique with total variation regularization and adaptive segmentation

V.V. Vlasov et al., J. Electron. Imaging 27: 043006 (2018)

$$\frac{1}{c^{e,f}} \frac{\partial \varphi^{e,f}(\mathbf{r}, t)}{\partial t} - \nabla \cdot [D^{e,f}(\mathbf{r}) \nabla \varphi^{e,f}(\mathbf{r}, t)] + [\mu_a^{e,f}(\mathbf{r}) + \mu_{af}(\mathbf{r})] \varphi^{e,f}(\mathbf{r}, t) = S^{e,f}(\mathbf{r}, t)$$

$$S^e(\mathbf{r}, t) = I_0 \delta(\mathbf{r} - \mathbf{r}_s) \delta(t - t_s)$$

$$S^f(\mathbf{r}, t) = \frac{\gamma(\mathbf{r}) \mu_{af}(\mathbf{r})}{\tau(\mathbf{r})} \int_{t_s}^t \varphi^e(\mathbf{r}, t') \exp\left(\frac{t' - t}{\tau(\mathbf{r})}\right) dt'$$

$$\varphi^{e,f}(\mathbf{r}_d, t) + 2AD^{e,f}(\mathbf{r}_d) \frac{\partial \varphi^{e,f}(\mathbf{r}_d, t)}{\partial q} = 0$$

# Our simplifying assumptions

- We use the asymptotic approximation for the fluorescence source function
- The contribution of fluorophore absorption is negligible
- Fluorescence quantum yield and lifetime are constant

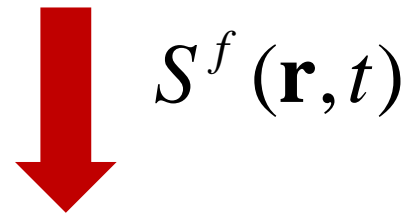
$$\frac{1}{c^{e,f}} \frac{\partial \varphi^{e,f}(\mathbf{r}, t)}{\partial t} - D^{e,f} \Delta \varphi^{e,f}(\mathbf{r}, t) + \mu_a^{e,f} \varphi^{e,f}(\mathbf{r}, t) = S^{e,f}(\mathbf{r}, t)$$

$$S^e(\mathbf{r}, t) = I_0 \delta(\mathbf{r} - \mathbf{r}_s) \delta(t - t_s)$$

$$S^f(\mathbf{r}, t) = \frac{\gamma \mu_{af}(\mathbf{r}) \cdot 4D^e c^e t^2}{\tau |\mathbf{r}|^2 + 4D^e c^e t^2} \varphi^e(\mathbf{r}, t)$$

# The constraint equation

$$\varphi^f(\mathbf{r}, t) = \int_{t_s}^t \int_V c^f S^f(\mathbf{r}', t') G^f(\mathbf{r} - \mathbf{r}', t - t') d^3 r' dt'$$



$$\varphi^f(\mathbf{r}, t) = c^f \gamma \int_{t_s}^t dt' \int_V \frac{\mu_{af}(\mathbf{r}') \cdot 4D^e c^e t'^2}{\tau |\mathbf{r}'|^2 + 4D^e c^e t'^2} \times \varphi^e(\mathbf{r}', t') G^f(\mathbf{r} - \mathbf{r}', t - t') d^3 r'$$

$$g(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = \frac{\Gamma^f(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}{\Gamma^e(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}$$

$$\Gamma^{e,f}(\mathbf{r}_d, t) = -c^{e,f} D^{e,f}(\mathbf{r}_d) \frac{\partial \varphi^{e,f}(\mathbf{r}_d, t)}{\partial q}$$

$$g(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = c^f \gamma \int_{t_s}^{t_d} dt \int_V \frac{\mu_{af}(\mathbf{r}) \cdot 4D^e c^e t^2}{\tau |\mathbf{r}|^2 + 4D^e c^e t^2}$$

$$\times \frac{\frac{\partial}{\partial q} G^f(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}, t_d - t)} \times \frac{G^e(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} d^3 r$$



- The scattering medium and the fluorescent inclusions have identical optical properties

$$c^e \cong c^f \cong c \quad \mu_a^e \cong \mu_a^f \cong \mu_a \quad D^e \cong D^f \cong D$$

- The Green function derivatives for the diffusion equations of exciting radiation and fluorescence are equal to each other

$$\frac{\partial G^f(\mathbf{r}_d - \mathbf{r}, t_d - t) / \partial q}{\partial G^e(\mathbf{r}_d - \mathbf{r}, t_d - t) / \partial q} \rightarrow 1$$

# Fundamental equation and sensitivity function

$$g(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = \int_V \left[ c\gamma \int_{t_s}^{t_d} \frac{4Dct^2}{\tau |\mathbf{r}|^2 + 4Dct^2} \frac{G^e(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} dt \right] \mu_{af}(\mathbf{r}) d^3 r$$

$$W_{\mu_{af}}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r})$$

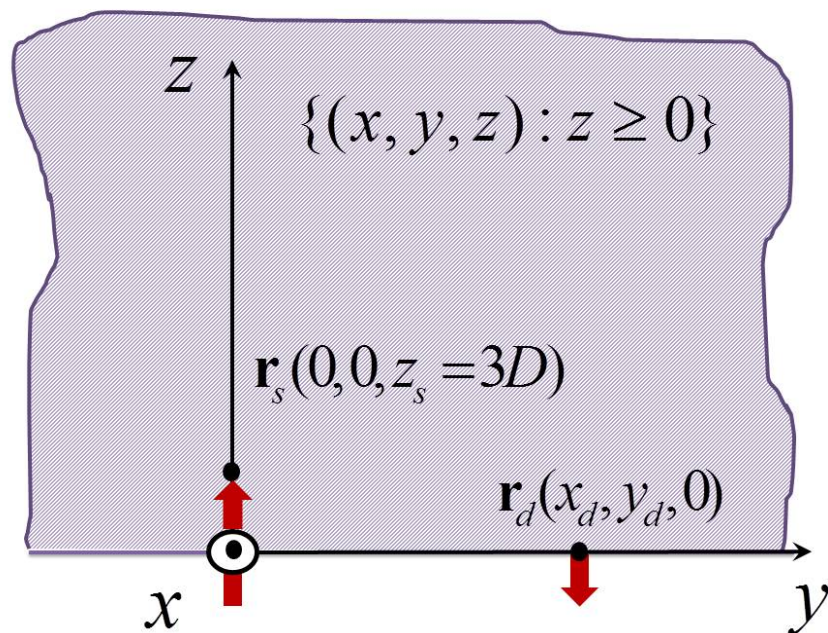
$$= c\gamma \int_{t_s}^{t_d} \frac{4Dct^2}{\tau |\mathbf{r}|^2 + 4Dct^2} \frac{G^e(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} dt$$

# Further simplification

$$W_{\mu_{af}}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = c\gamma \int_{t_s}^{t_d} \frac{1}{\frac{\tau}{4Dc} \frac{|\mathbf{r}|^2}{t^2} + 1} \frac{G^e(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} dt$$

$\frac{|\mathbf{r}|^2}{t^2}$  can be changed by  $\frac{|\mathbf{r}_d|^2}{t_d^2}$

$$W_{\mu_{af}}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = \frac{4\gamma Dc^2 t_d^2}{\tau |\mathbf{r}_d|^2 + 4Dct_d^2} \int_{t_s}^{t_d} \frac{G^e(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial q} G^e(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} dt$$



$$t_s = 0$$

$$\varphi^{e,f}(\mathbf{r}_d, t) = 0$$

$$G(\mathbf{r} - \mathbf{r}', t - t') = [4\pi Dc(t - t')]^{-3/2} \exp[-\mu_a c(t - t')] \\ \times \left\{ \exp\left[-\frac{(x - x')^2 + (y - y')^2 + (z - z')^2}{4Dc(t - t')}\right] - \exp\left[-\frac{(x - x')^2 + (y - y')^2 + (z + z')^2}{4Dc(t - t')}\right] \right\}$$

$$I = \int_0^{t_d} \frac{G(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial q} G(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial q} G(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} dt$$

$$I = I_- - I_+, \quad I_{\pm} = \frac{z}{\pi(4Dc)^{3/2} t_d^{1/2} z_s} \exp \left[ \frac{x_d^2 + y_d^2 + z_s^2}{4Dct_d} - \left( \sqrt{p} + \sqrt{q_{\pm}} \right)^2 \right] \\ \times \left( q_{\pm}^{-1/2} + 2p^{-1/2} + \frac{1}{2} p^{-3/2} + p^{-1} q_{\pm}^{1/2} \right),$$

$$p = \frac{(x - x_d)^2 + (y - y_d)^2 + z^2}{4Dct_d}, \quad q_{\pm} = \frac{x^2 + y^2 + (z \pm z_s)^2}{4Dct_d}$$

A.B. Konovalov, V.V. Vlasov, Quantum Electron. 44: 719 (2014)

A.B. Konovalov, V.V. Vlasov, Proc. PIERS Spring: 3487 (2017)

# Analytic representation for sensitivity function



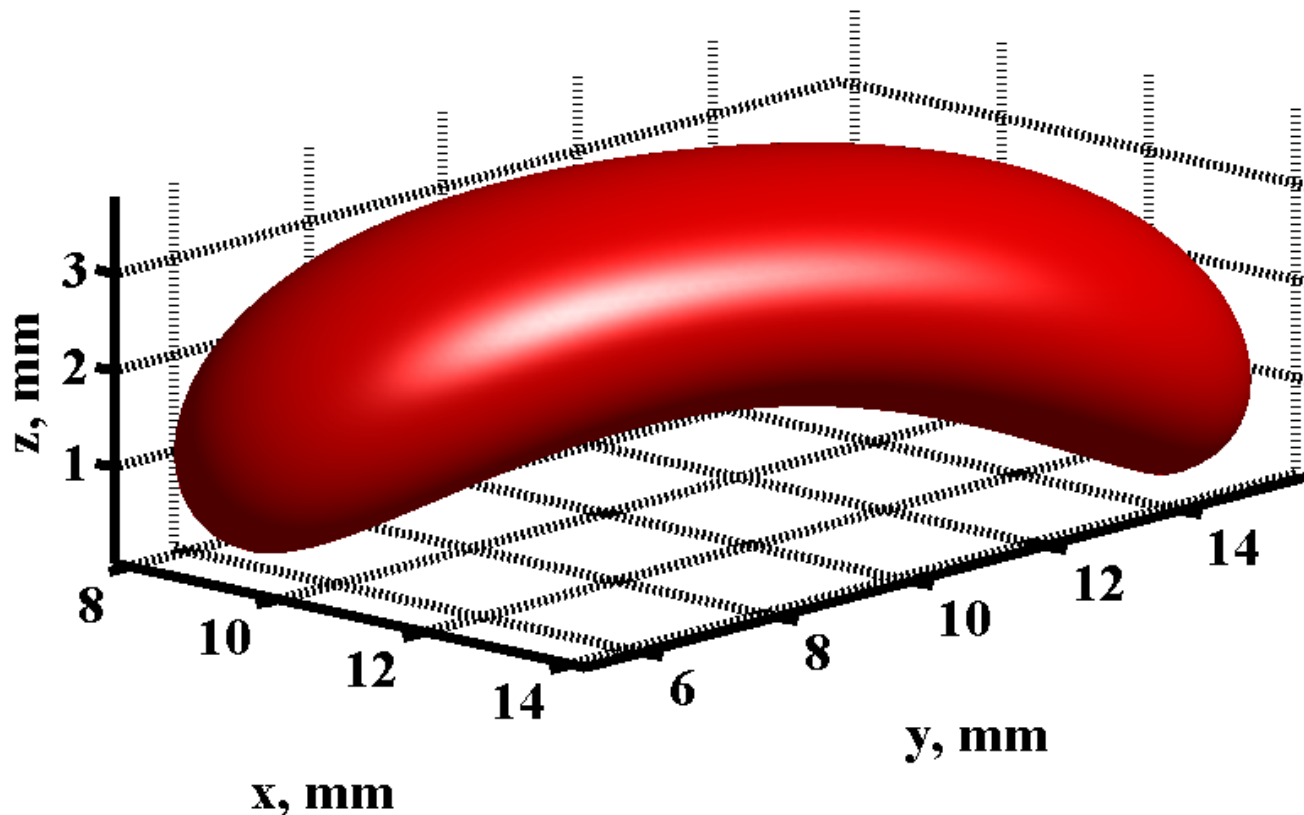
$$W_{\mu_{af}}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = \left(W_{\mu_{af}}\right)_- - \left(W_{\mu_{af}}\right)_+,$$

$$\left(W_{\mu_{af}}\right)_\pm = \frac{\gamma z}{24\pi D^{5/2} (ct_d)^{1/2}} \cdot \frac{4Dct_d^2}{\tau(x_d^2 + y_d^2) + 4Dct_d^2} \\ \times \exp\left[\frac{x_d^2 + y_d^2 + (3D)^2}{4Dct_d} - \left(\sqrt{p} + \sqrt{q_\pm}\right)^2\right] \left(q_\pm^{-1/2} + 2p^{-1/2} + \frac{1}{2}p^{-3/2} + p^{-1}q_\pm^{1/2}\right),$$

$$p = \frac{(x - x_d)^2 + (y - y_d)^2 + z^2}{4Dct_d}, \quad q_\pm = \frac{x^2 + y^2 + (z \pm 3D)^2}{4Dct_d}$$

# Example of sensitivity function visualization

Source and receiver coordinates in mm:  
 $x_s=9$ ;  $y_s=6$ ;  $x_d=13$ ;  $y_d=15$



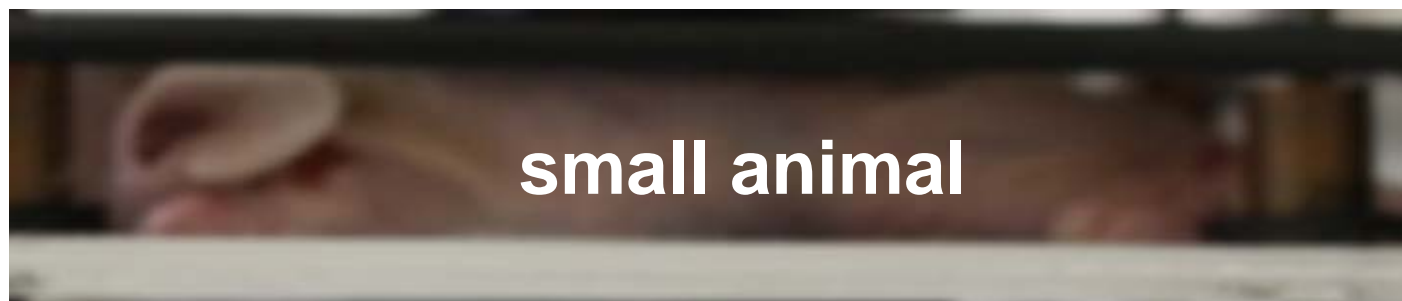
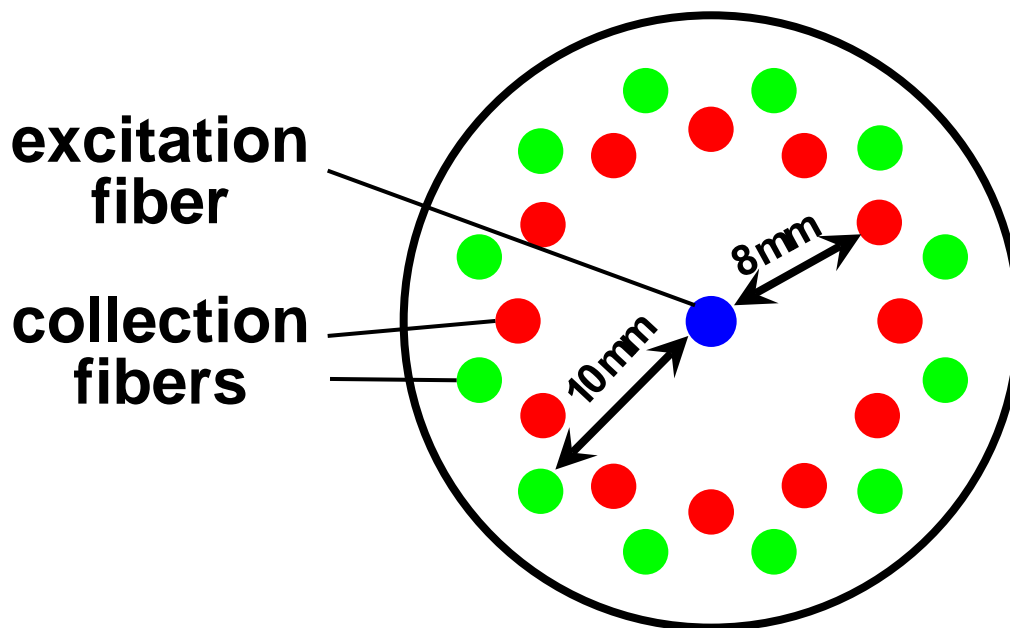
$$c = 0.214 \text{ mm / ps} \quad D = 0.194 \text{ mm} \quad \gamma = 1 \quad \tau = 1000 \text{ ps}$$

$$g_{i,j} = \sum_{m=1}^M \sum_{n=1}^N \sum_{l=1}^L W_{m,n,l}^{i,j} f_{m,n,l} \quad (\mathbf{g} = \mathbf{Wf})$$

$$\begin{aligned} (W_{m,n,l}^{i,j})_{\pm} = & \frac{\Delta^3 \gamma z_l}{24\pi D^{5/2} (ct_d)^{1/2}} \cdot \frac{4Dct_d^2}{\tau(x_i^2 + y_i^2) + 4Dct_d^2} \cdot \exp\left[\frac{x_i^2 + y_i^2 + (3D)^2}{4Dct_d}\right] \\ & - \left[ \sqrt{\frac{(x_n - x_i)^2 + (y_m - y_i)^2 + z_l^2}{4Dct_d}} + \sqrt{\frac{(x_n - x_j)^2 + (y_m - y_j)^2 + (z_l \pm 3D)^2}{4Dct_d}} \right]^2 \\ & \times \left\{ \left[ \frac{(x_n - x_j)^2 + (y_m - y_j)^2 + (z_l \pm 3D)^2}{4Dct_d} \right]^{-1/2} + 2 \left[ \frac{(x_n - x_i)^2 + (y_m - y_i)^2 + z_l^2}{4Dct_d} \right]^{-1/2} \right. \\ & \left. + \frac{1}{2} \left[ \frac{(x_n - x_i)^2 + (y_m - y_i)^2 + z_l^2}{4Dct_d} \right]^{-3/2} + \left[ \frac{(x_n - x_i)^2 + (y_m - y_i)^2 + z_l^2}{4Dct_d} \right]^{-1} \right. \\ & \left. \times \left[ \frac{(x_n - x_j)^2 + (y_m - y_j)^2 + (z_l \pm 3D)^2}{4Dct_d} \right]^{1/2} \right\} \end{aligned}$$

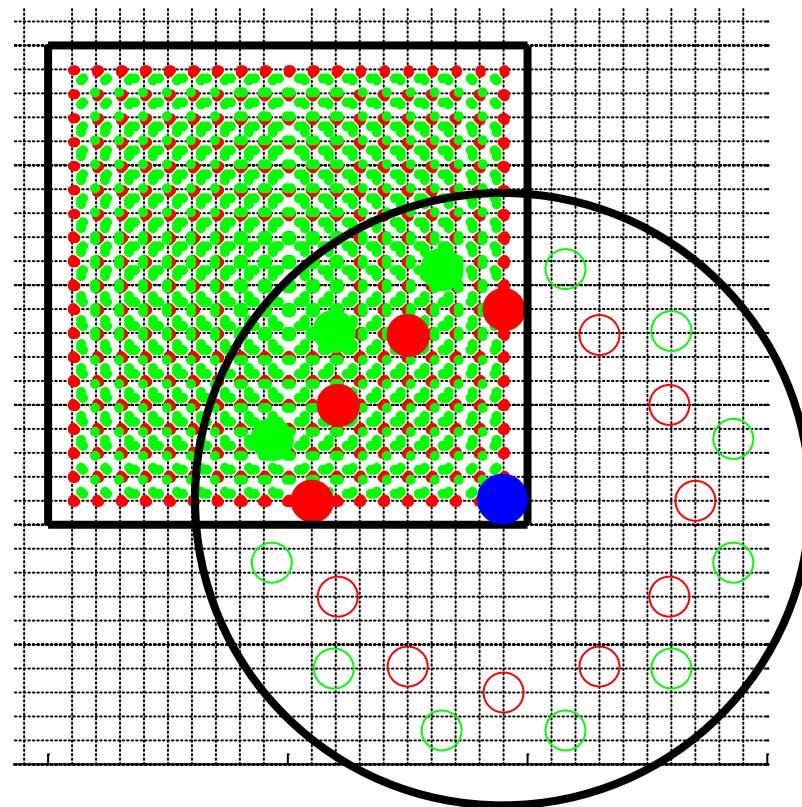
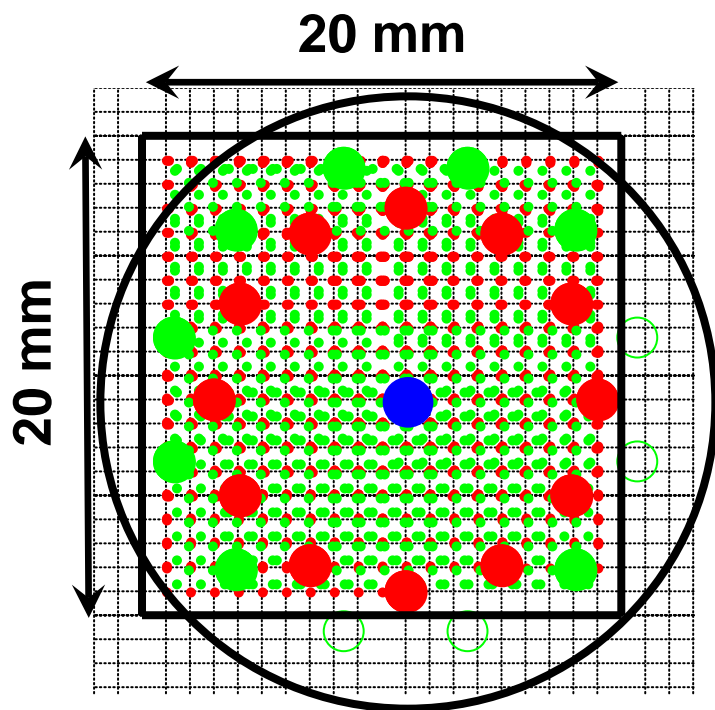


# Virtual fluorescent tomograph



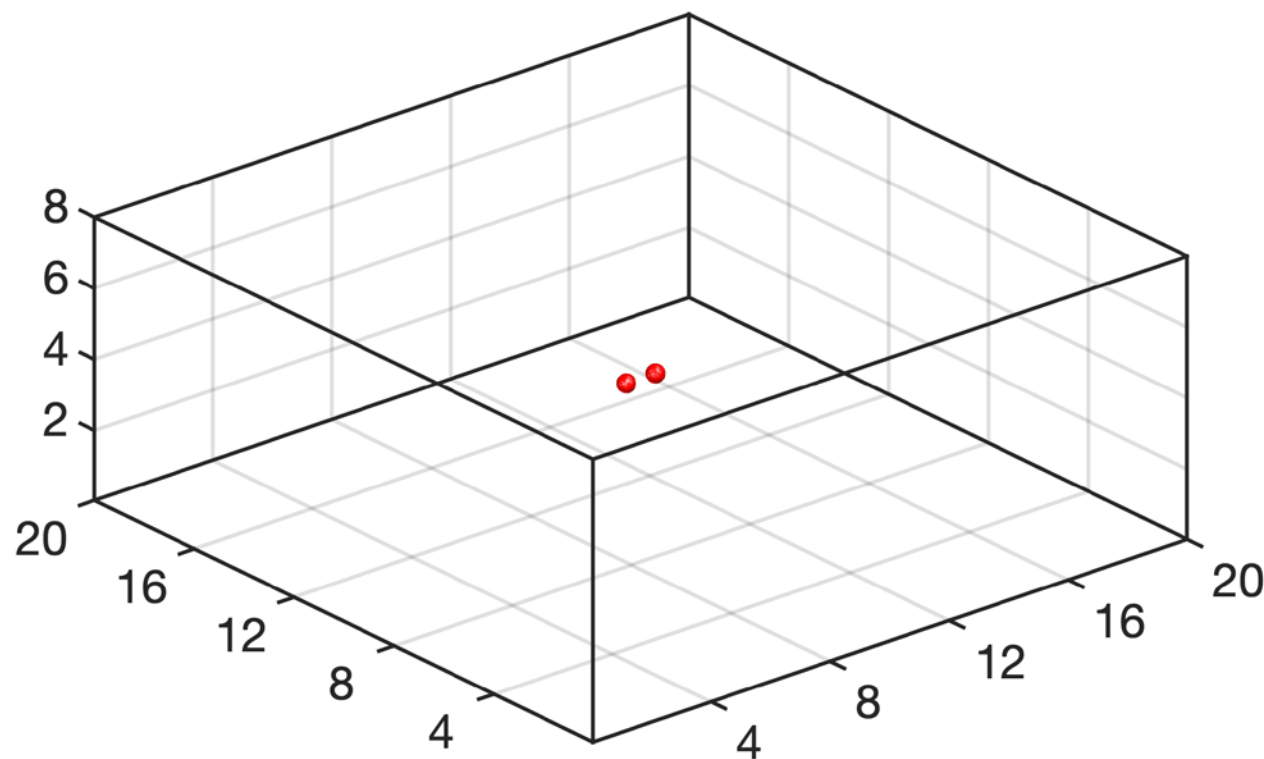
E. Cordero et al., J. Biomed. Opt. 23: 071210 (2018)

# Scanning of the object



**1419 useful source-receiver connections**

# The object to be reconstructed



$$c = 0.214 \text{ mm / ps}$$

$$D = 0.194 \text{ mm}$$

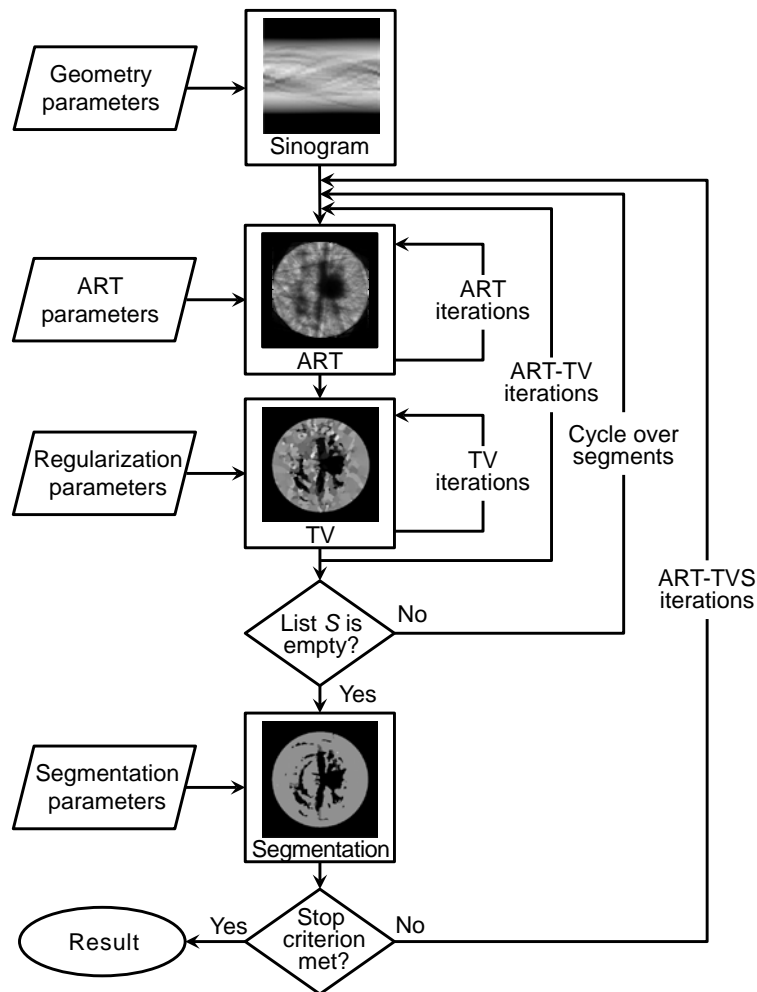
$$\gamma = 1$$

$$\tau = 1000 \text{ ps}$$

$$\mu_{af} = 0.01 \text{ mm}^{-1}$$

**The values of time gates are 100 and 150 ps.  
They correspond to the source-receiver  
separations of 8 and 10 millimeters, respectively.**

# The ART-TVS algorithm



$$\text{ART-TVS} = \text{ART-TV} + \text{S}$$

**Algebraic reconstruction  
with total variation  
regularization (ART-TV)**

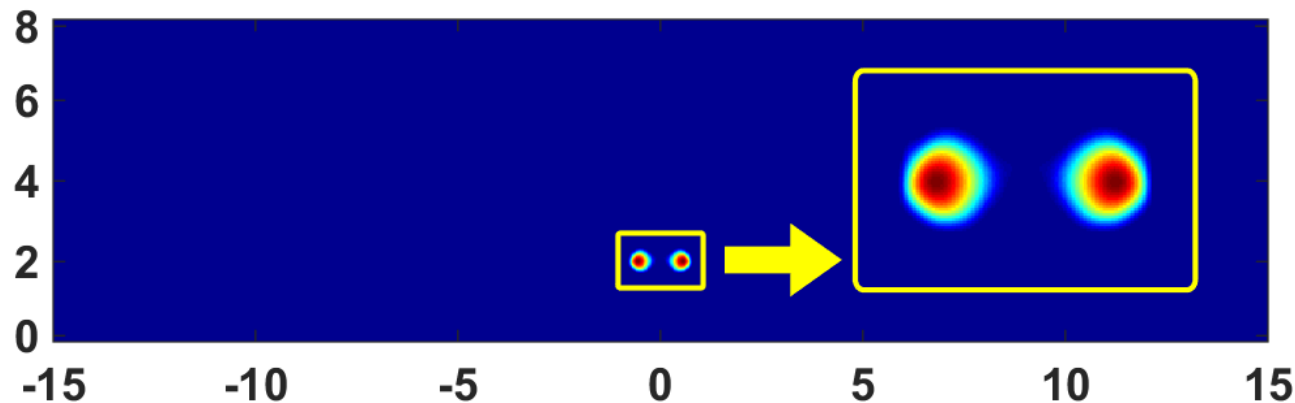
H. Yu, G. Wang, *Phys. Med. Biol.* 54,  
2791 (2009)

**Adaptive segmentation (S)  
based on region growing**

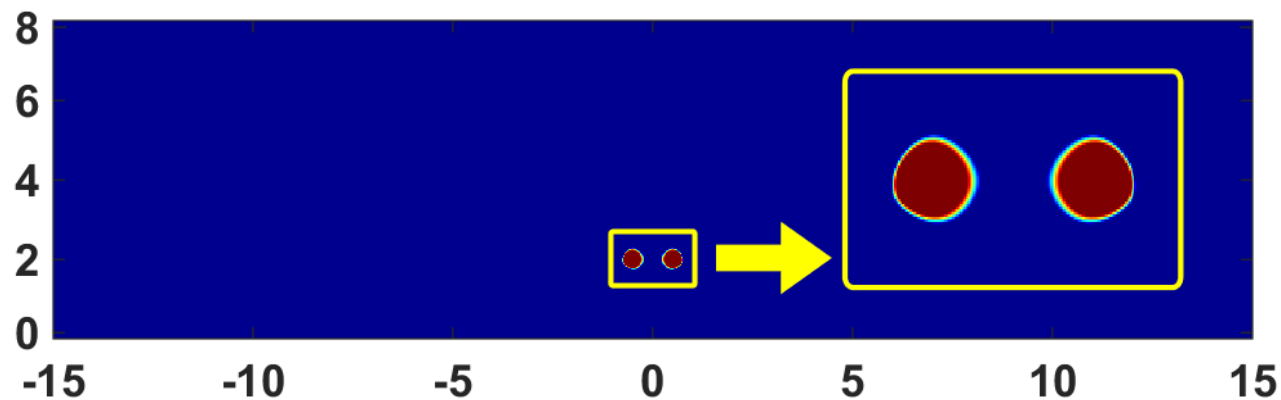
A. Mehnert, O. Jackway, *Pattern  
Recognit. Lett.* 18, 1065 (1997)

V.V. Vlasov et al., *J. Electron. Imaging* 27: 043006 (2018)

# The main advantage of ART-TVS



**ART**

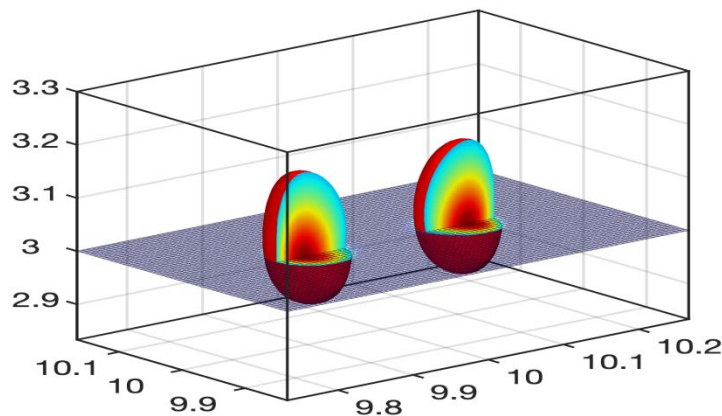


**ART-TVS**

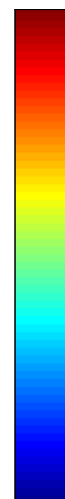
# The results of 3D reconstruction

depth of 3 mm

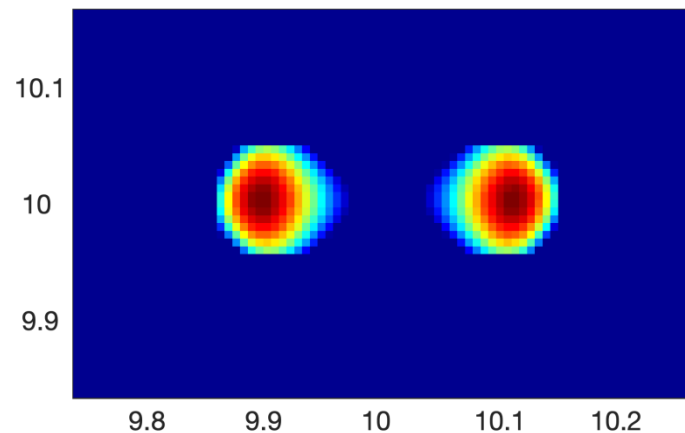
0.1 mm



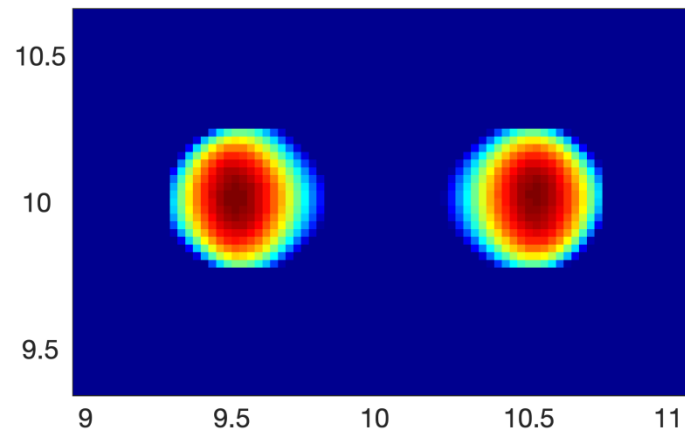
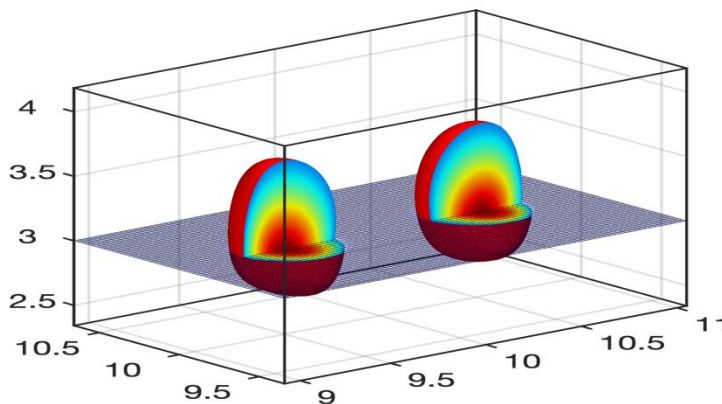
0.01 mm<sup>-1</sup>



0



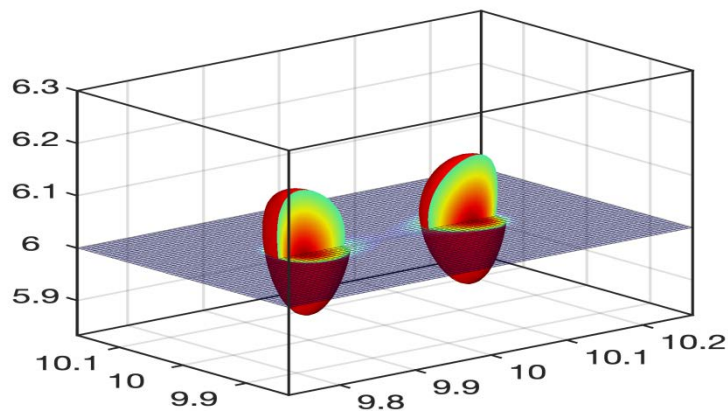
0.5 mm



# The results of 3D reconstruction

depth of 6 mm

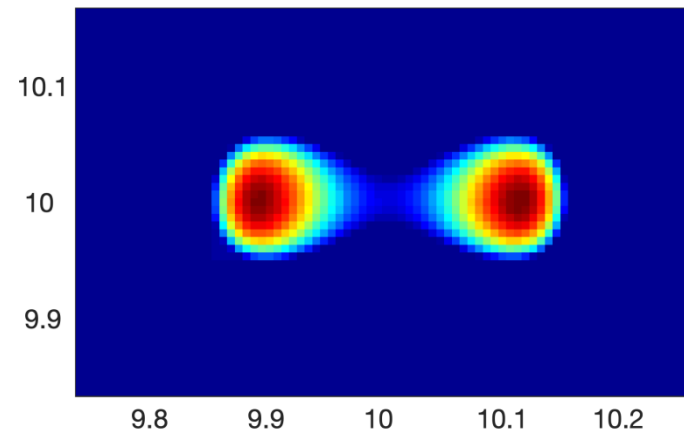
0.1 mm



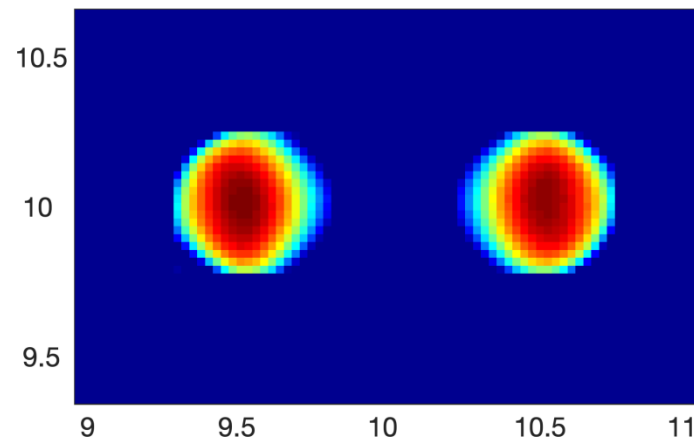
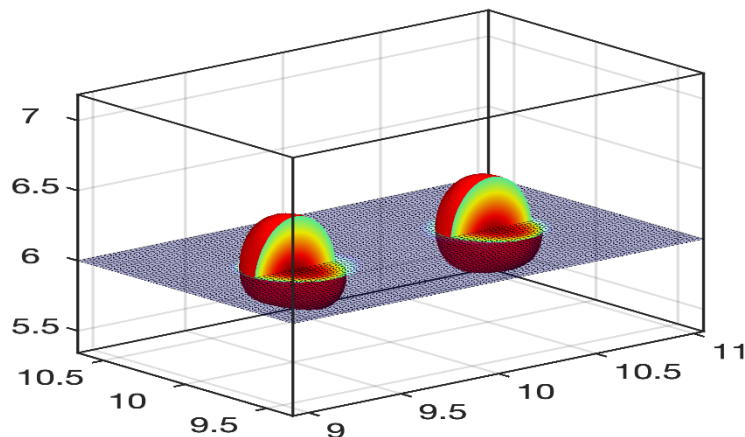
0.01 mm<sup>-1</sup>



0

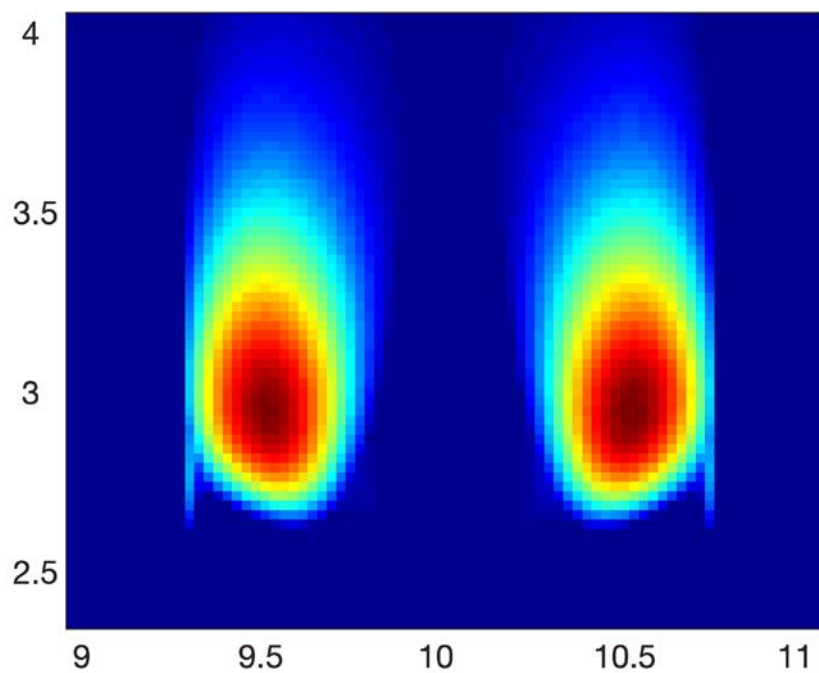


0.5 mm

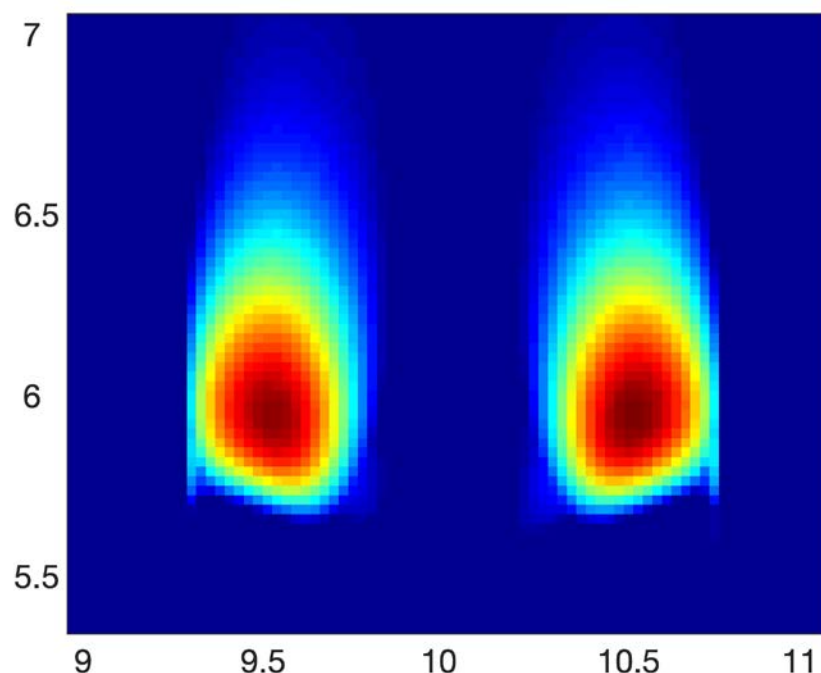


# The results of 3D reconstruction

## depth of 3 mm



## depth of 6 mm








# Conclusion and further research

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- Our approach to macroscopic FMT allows the resolution of 100 micrometers to be obtained
- Our further research is aimed at developing a physical experiment to verify the results
- Of special interest to us is to adapt our approach to fluorescence lifetime tomography

**Thank you for your time!**



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