



Russian Federal Nuclear Center –
Zababakhin Institute of Applied Physics



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An equivalent inverse source method of evaluating the weight functions for parallel-plate time-domain diffuse optical tomography

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- 1. Introduction**
- 2. Analytical representation of the weight functions for half-space**
- 3. Finding the positions of the equivalent and equivalent inverse sources**
- 4. Numerical experiment on reconstruction of optical inhomogeneities**
- 5. Resolution analysis and conclusions**

➤ The fundamental equation

$$g(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = \int_V [W_{\mu_a}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) \delta\mu_a(\mathbf{r}) + W_D(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) \delta D(\mathbf{r})] d^3 r,$$

$$g(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = \frac{\Gamma_0(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d} - \Gamma(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}{\Gamma_0(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}} \quad \text{is the time-resolved optical projection,}$$

$\Gamma(\mathbf{r}_s, t_s, \mathbf{r}_d, t)$ is the temporal point spread function

➤ The weight functions

$$W_{\mu_a}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = c \int_{t_s}^{t_d} \frac{G(\mathbf{r} - \mathbf{r}_s, t - t_s) \partial G(\mathbf{r}_d - \mathbf{r}, t_d - t) / \partial \eta}{\partial G(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s) / \partial \eta} dt$$

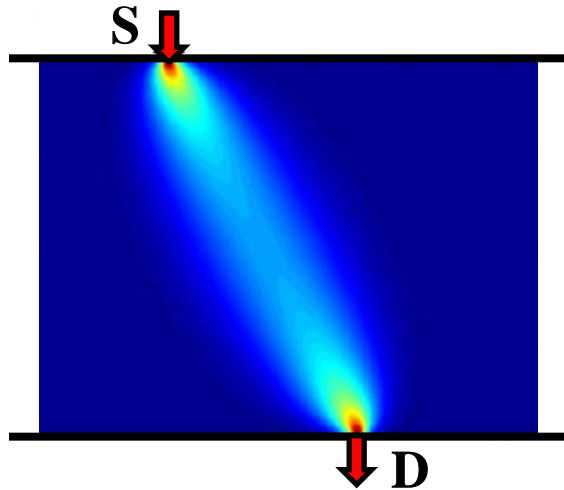
$$W_D(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = -\frac{1}{D} \int_{t_s}^{t_d} \frac{G(\mathbf{r} - \mathbf{r}_s, t - t_s) \partial G(\mathbf{r}_d - \mathbf{r}, t_d - t) / \partial \eta}{\partial G(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s) / \partial \eta} \left[c\mu_a + \frac{\partial}{\partial t} \ln G(\mathbf{r} - \mathbf{r}_s, t - t_s) \right] dt$$

V.V. Lyubimov, *Opt. Spectrosc.* 80: 616 (1996)

A.B. Konovalov et al., *Proc. SPIE* 8088: 80880T (2011)

Two-step approach for weight function evaluation

□ Our approach is based on two assumptions



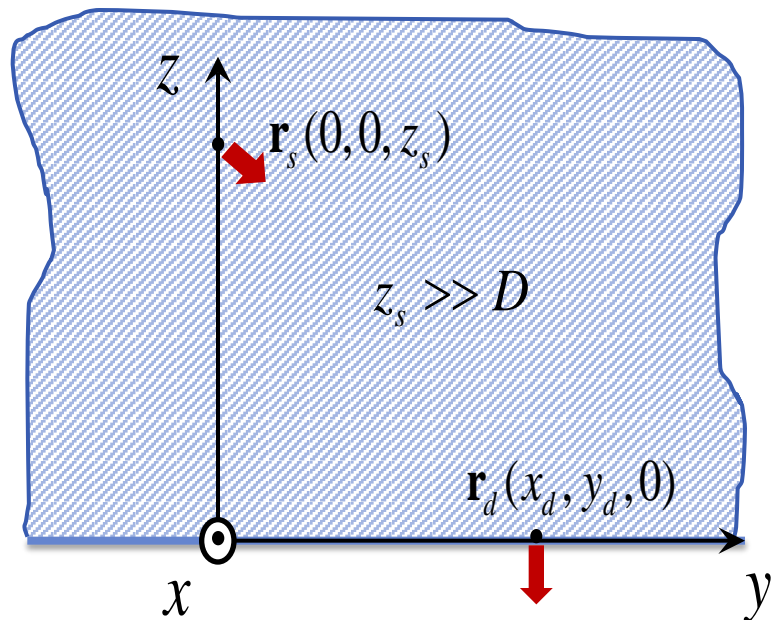
- The effect of one boundary on photon migration near the other boundary is negligibly small.
- The distributions of photons near the source S on one boundary and near the receiver D on the other boundary are similar in nature.

□ Our approach involves two steps

- Derive the analytical expressions for the case of semi-infinite scattering medium
- Apply them to obtain the weight functions for the flat layer using the equivalent inverse source method

3D case: half-space

$$\{(x, y, z) : z \geq 0\}$$



$$W_{\mu_a}(\dots) = c \int_{t_s}^{t_d} \frac{\mathbf{G}(\dots) \partial \mathbf{G}(\dots) / \partial \eta}{\partial \mathbf{G}(\dots) / \partial \eta} dt$$

$$W_D(\dots) = -\frac{1}{D} \int_{t_s}^{t_d} \frac{\mathbf{G}(\dots) \partial \mathbf{G}(\dots) / \partial \eta}{\partial \mathbf{G}(\dots) / \partial \eta} \times \left[c\mu_a + \frac{\partial}{\partial t} \ln \mathbf{G}(\dots) \right] dt$$

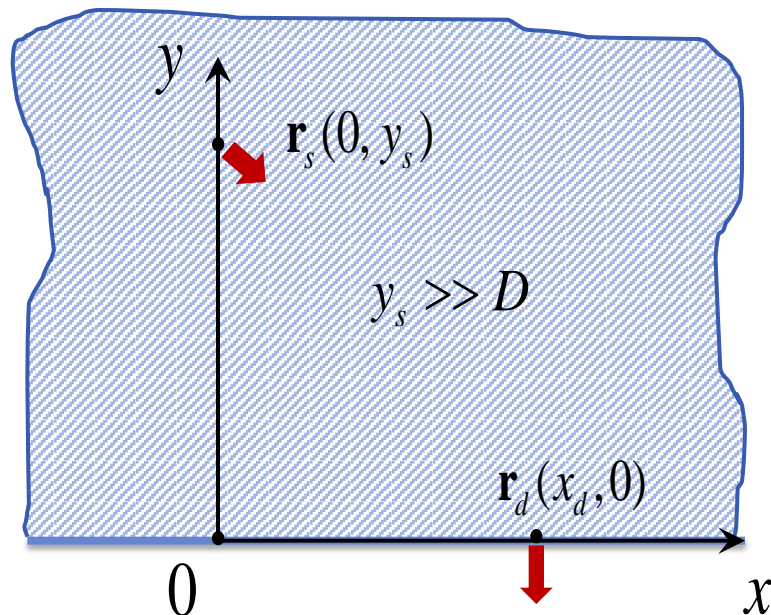
3D Green's function

$$\mathbf{G}^{3D}(\mathbf{r} - \mathbf{r}', t - t') = [4\pi Dc(t - t')]^{-3/2} \exp[-\mu_a c(t - t')]$$

$$\times \left\{ \exp\left[-\frac{(x-x')^2 + (y-y')^2 + (z-z')^2}{4Dc(t-t')}\right] - \exp\left[-\frac{(x-x')^2 + (y-y')^2 + (z+z')^2}{4Dc(t-t')}\right] \right\}$$

2D case: half-plane

$$\{(x, y) : y \geq 0\}$$



$$W_{\mu_a}(\dots) = c \int_{t_s}^{t_d} \frac{\mathbf{G}(\dots) \partial \mathbf{G}(\dots) / \partial \eta}{\partial \mathbf{G}(\dots) / \partial \eta} dt$$

$$W_D(\dots) = -\frac{1}{D} \int_{t_s}^{t_d} \frac{\mathbf{G}(\dots) \partial \mathbf{G}(\dots) / \partial \eta}{\partial \mathbf{G}(\dots) / \partial \eta} \times \left[c\mu_a + \frac{\partial}{\partial t} \ln \mathbf{G}(\dots) \right] dt$$

2D Green's function

$$\mathbf{G}^{2D}(\mathbf{r} - \mathbf{r}', t - t') = [4\pi Dc(t - t')]^{-1} \exp[-\mu_a c(t - t')] \times \left\{ \exp\left[-\frac{(x - x')^2 + (y - y')^2}{4Dc(t - t')} \right] - \exp\left[-\frac{(x - x')^2 + (y + y')^2}{4Dc(t - t')} \right] \right\}$$

$W_{\mu_a}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = W_{\mu_a}^- - W_{\mu_a}^+$, $W_D(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = W_D^+ - W_D^-$, **where**

$$W_{\mu_a}^{\pm} = \frac{z}{\pi D z_s} \exp\left[\frac{x_d^2 + y_d^2 + z_s^2 - (\gamma \pm \beta_{\pm})^2}{4Dct_d}\right] \left[\frac{1}{4\beta_{\pm}} \left(1 \pm \frac{\beta_{\pm}}{\gamma}\right)^2 + \frac{Dct_d}{2\gamma^3} \right],$$

$$W_D^{\pm} = \frac{z}{\pi D z_s} \exp\left[\frac{x_d^2 + y_d^2 + z_s^2 - (\gamma^2 \pm \beta_{\pm}^2)^2}{4Dct_d}\right] \left[\frac{\gamma^2}{16D^2c^2t_d^2\beta_{\pm}} \left(1 \pm \frac{\beta_{\pm}}{\gamma}\right)^4 + \frac{1}{8Dct_d\beta_{\pm}} \left(\frac{\beta_{\pm}^3}{\gamma^3} - 3\frac{\beta_{\pm}^2}{\gamma^2} - 9\frac{\beta_{\pm}}{\gamma} - 5 \right) - \frac{3}{4\gamma^3} \right],$$

$$\gamma = \sqrt{(x - x_d)^2 + (y - y_d)^2 + z^2}, \quad \beta_{\pm} = \sqrt{x^2 + y^2 + (z \pm z_s)^2}$$

A.B. Konovalov, V.V. Vlasov, *Quantum Electron.* 44: 719 (2014)

A.B. Konovalov, V.V. Vlasov, *Proc. SPIE* 9917: 99170S (2016)

$W_{\mu_a}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = W_{\mu_a}^- - W_{\mu_a}^+$, $W_D(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) = W_D^+ - W_D^-$, **where**

$$W_{\mu_a}^{\pm} = \frac{y}{2y_s} \sqrt{\frac{ct_d}{\pi D}} \exp\left[\frac{x_d^2 + y_s^2 - (\gamma + \beta_{\pm})^2}{4Dct_d}\right] \left[\frac{1}{\sqrt{\gamma\beta_{\pm}}} + \frac{\sqrt{\beta_{\pm}}}{\gamma^{3/2}} \right],$$

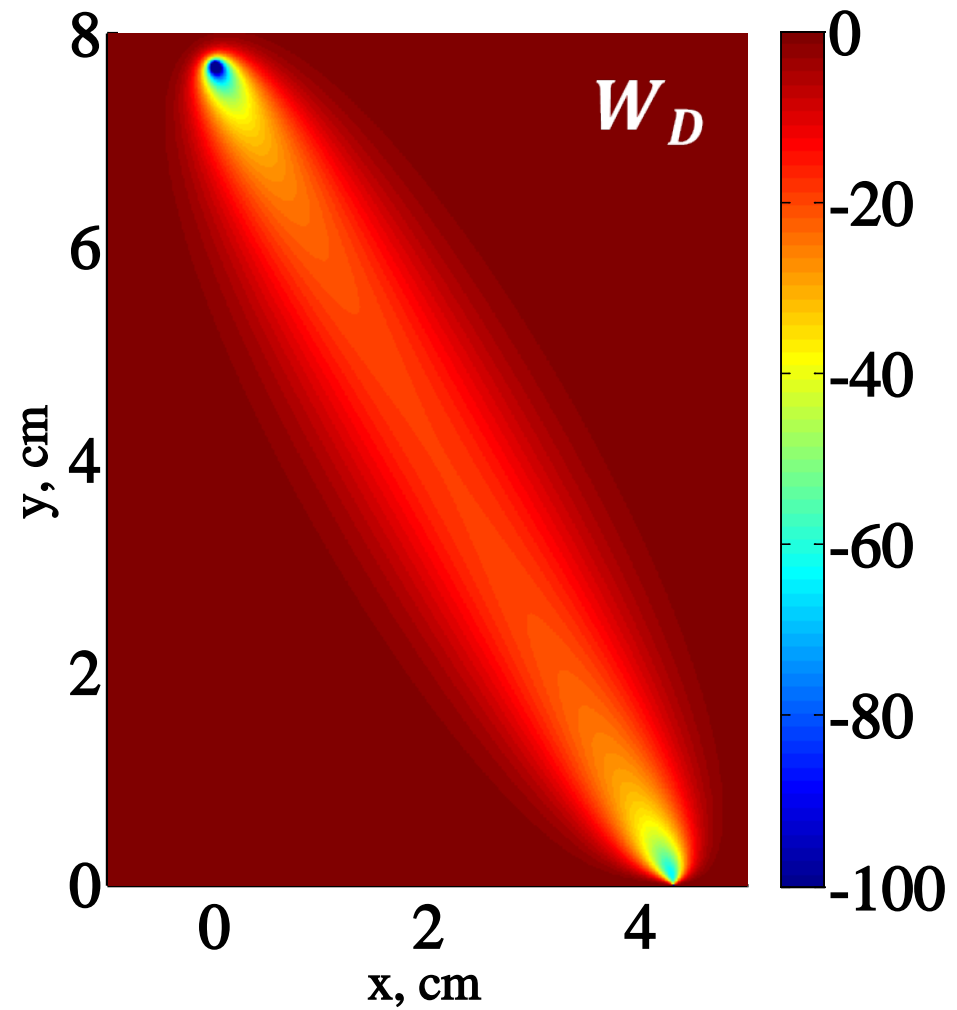
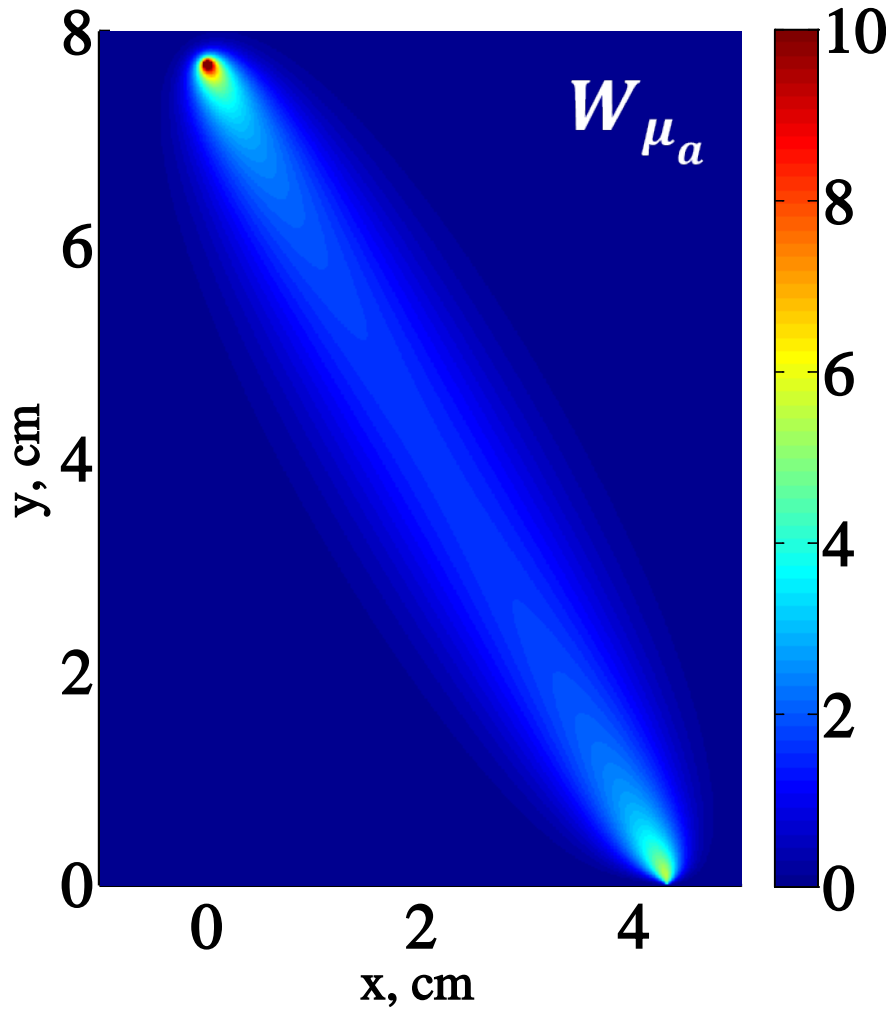
$$W_D^{\pm} = \frac{y}{D(4\pi Dct_d)^{3/2} y_s} \exp\left[\frac{x_d^2 + y_s^2 - (\gamma + \beta_{\pm})^2}{4Dct_d}\right] \times \left[\frac{1}{\sqrt{\gamma\beta_{\pm}}} (\gamma^2 + 3\beta_{\pm}^2 - 8Dct_d) + \frac{\sqrt{\beta_{\pm}}}{\gamma^{3/2}} (3\gamma^2 + \beta_{\pm}^2 - 4Dct_d) \right],$$

$$\gamma = \sqrt{(x - x_d)^2 + y^2}, \quad \beta_{\pm} = \sqrt{x^2 + (y \pm y_s)^2}$$

A.B. Konovalov, V.V. Vlasov, *Quantum Electron.* 44: 719 (2014)

A.B. Konovalov, V.V. Vlasov, *Proc. SPIE* 9917: 99170S (2016)

Examples of the weight functions

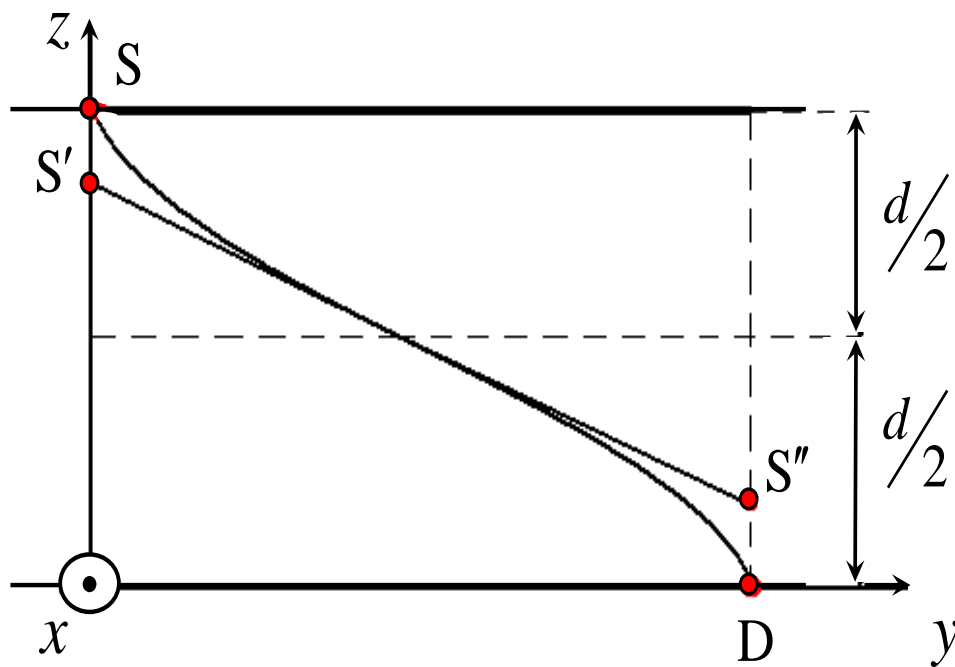


$$D = 0.0332 \text{ cm}$$

$$c = 0.0214 \text{ cm / ps}$$

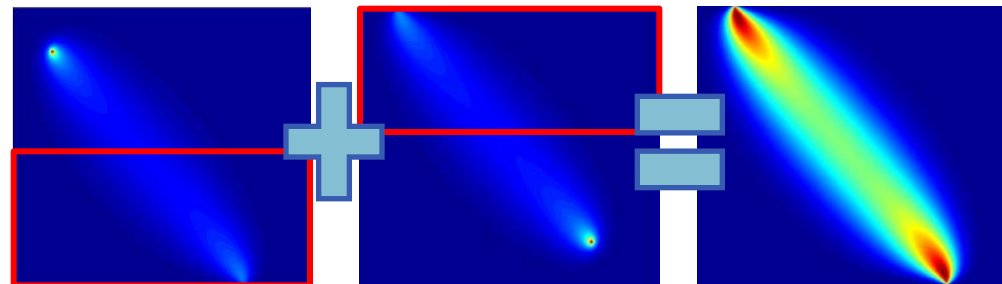
$$t_d = 1000 \text{ ps}$$

Method of the equivalent inverse source



- Find the position of S' inside the flat layer and calculate the weight function for one half of the layer.
- Find the position of S'' and calculate the weight function for the other half of the layer.

- Perform superposition of the useful halves to obtain the weight function for the full layer.



Finding the positions of the equivalent sources

The position of the equivalent source S' and the position of the equivalent inverse source S'' are found from relations for the photon average trajectories.

- The coordinate $z_{S'}$ can be found by solving the equation

$$Z|_{t=t_d/2} = d/2, \quad \text{where}$$

$$Z(t) = \left[\frac{2Dct}{z_{S'}} + \frac{z_{S'}(t_d - t)}{t_d} \right] \operatorname{erf} \left[\frac{z_{S'}^2(t_d - t)}{4Dc t t_d} \right]^{1/2} + \left[\frac{4Dct(t_d - t)}{\pi t_d} \right]^{1/2} \exp \left[-\frac{z_{S'}^2(t_d - t)}{4Dc t t_d} \right],$$

$\operatorname{erf}(\xi)$ is the error function

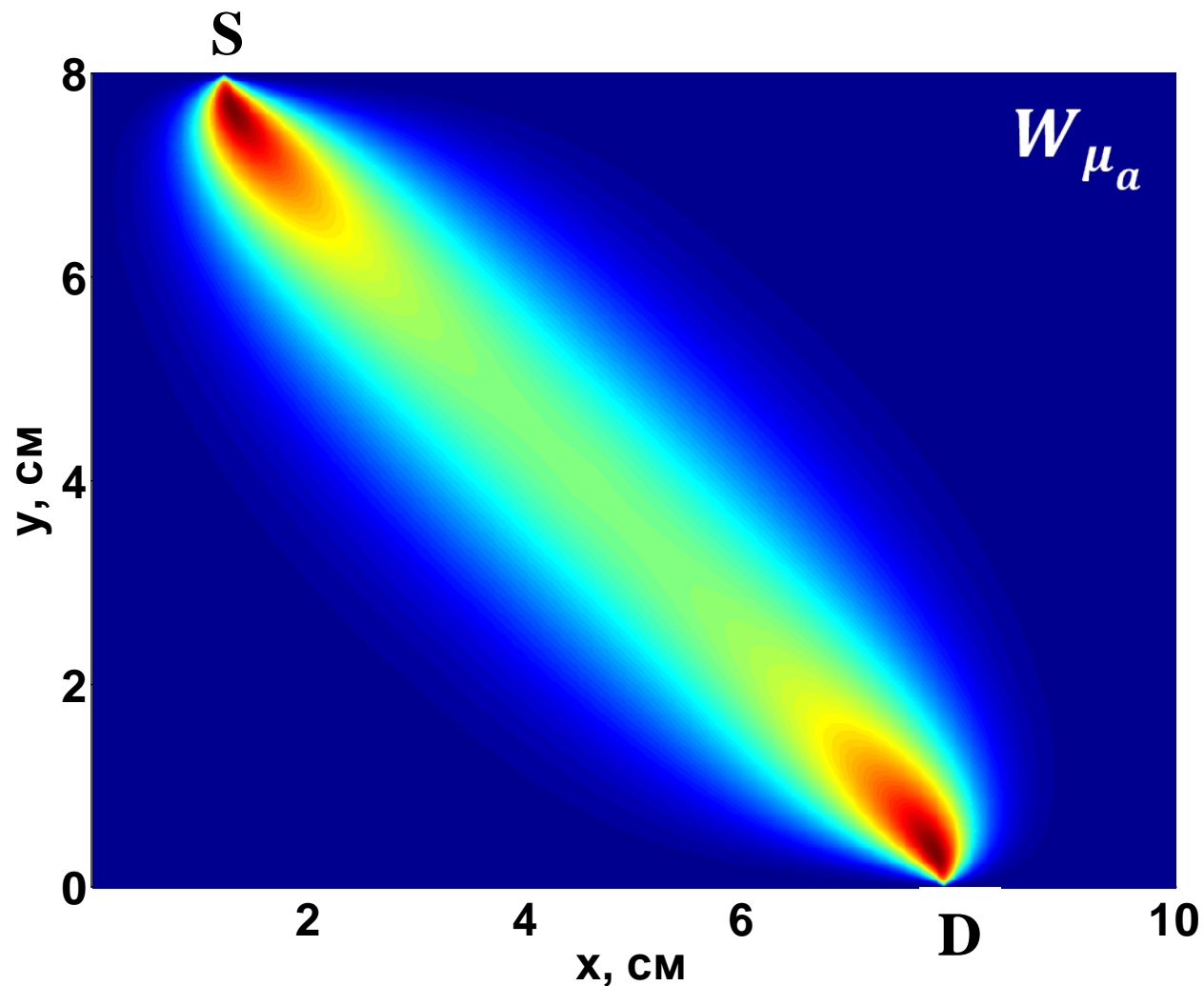
- For the coordinate $z_{S''}$ we will have

$$z_{S''} = d - z_{S'}$$

A.B. Konovalov et al., Quantum Electron. 36: 1048 (2006)

A.B. Konovalov et al., Optik 124: 6000 (2013)

The weight function for a 2D flat layer



$$D = 0.0332 \text{ cm}$$

$$c = 0.0214 \text{ cm / ps}$$

$$t_d = 1000 \text{ ps}$$

$$\mathbf{r}_s (1.2, 8.0 \text{ cm})$$

$$\mathbf{r}_d (7.8 \text{ cm}, 0)$$

The reconstruction problem statement

The reconstruction problem is reduced to the solution of the following system of linear algebraic equations.

$$\begin{pmatrix} \mathbf{W}_{\mu_a} & \mathbf{W}_D \end{pmatrix} \begin{pmatrix} \delta\mu_a \\ \delta\mathbf{D} \end{pmatrix} = \mathbf{g}, \quad \text{where}$$

$\begin{pmatrix} \mathbf{W}_{\mu_a} & \mathbf{W}_D \end{pmatrix}$ is the weight matrix obtained by sampling and combining all weight functions calculated for different positions of sources and receivers

$\begin{pmatrix} \delta\mu_a \\ \delta\mathbf{D} \end{pmatrix}$ is the vector of unknown local disturbances of the absorption and diffusion coefficients

\mathbf{g} is the vector of time-resolved optical projections

Our reconstruction algorithm

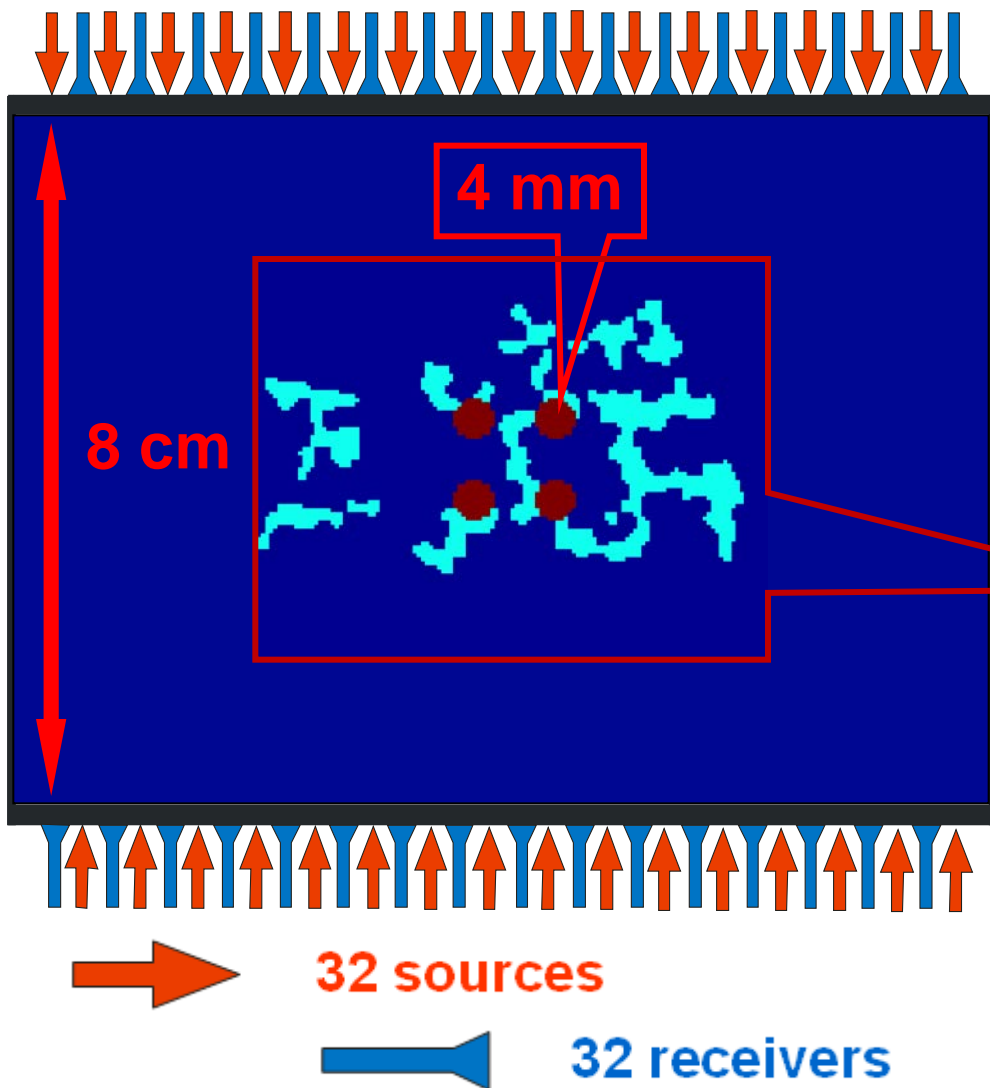
To solve SLAE we use an algorithm that combines the algebraic reconstruction technique (ART) with regularization by total variation (TV) norm minimization.



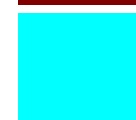
Outline of the algorithm

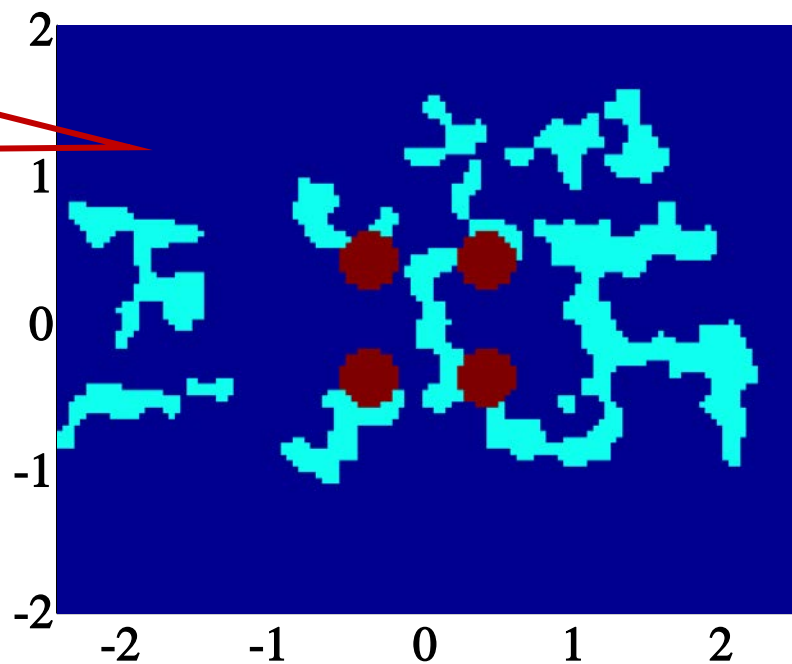
- **Step 1**: Do a number of ART iterations
- **Step 2**: Process the result through TV-norm minimization
- **Step 3**: Check the stop criterion. Go to **Step 1** if not satisfied
- **Step 4**: Stop

The researcher interactively chooses when ART iterations should stop and TV-processing start. For the stop criterion, we use the iteration convergence rate.

The numerical phantom for study



	$\mu_a = 0.05 \text{ cm}^{-1}$ $D = 0.0332 \text{ cm}$
	$\mu_a = 0.075 \text{ cm}^{-1}$ $D = 0.0255 \text{ cm}$
	$\mu_a = 0.06 \text{ cm}^{-1}$ $D = 0.0302 \text{ cm}$

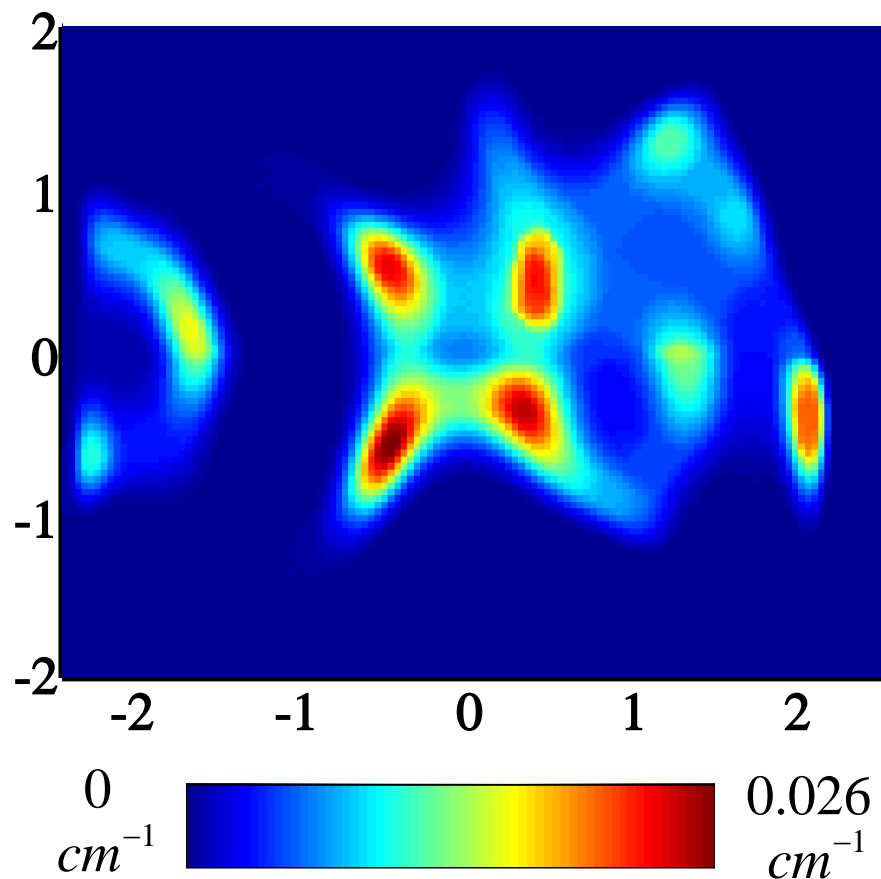


The optical parameters we chose

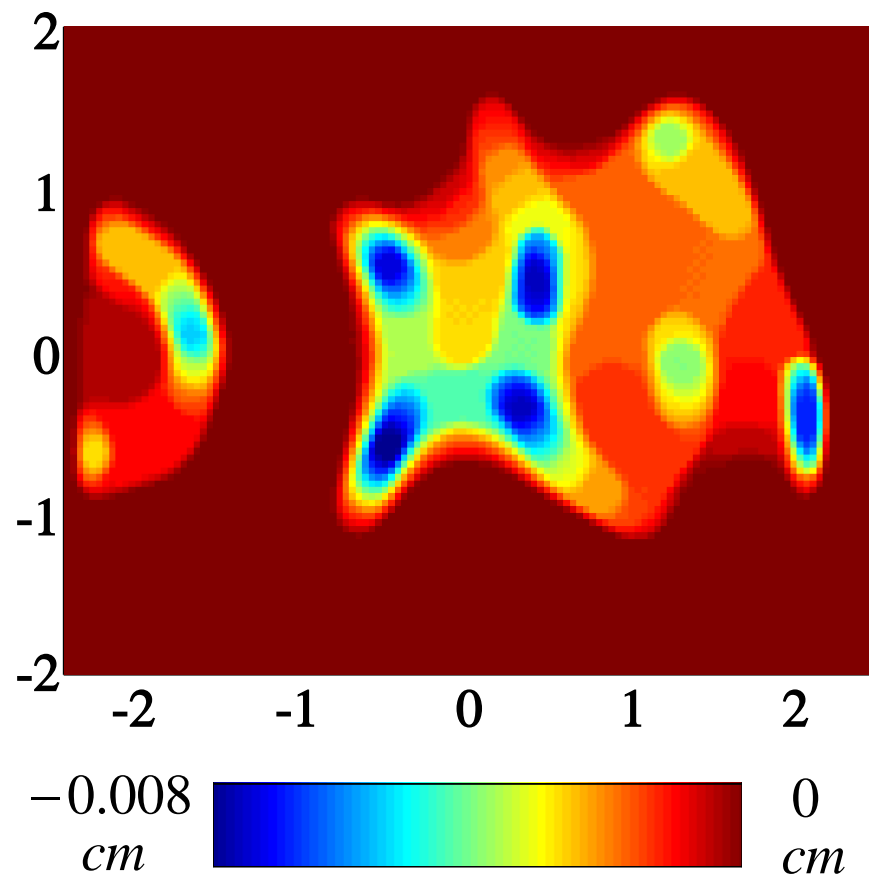
Tissue	c <i>cm/ ps</i>	μ_a <i>cm⁻¹</i>	$\delta\mu_a$ <i>cm⁻¹</i>	μ'_s <i>cm⁻¹</i>	$\delta\mu'_s$ <i>cm⁻¹</i>	D <i>cm</i>	δD <i>cm</i>
Fat	0.0214	0.050	0	10	0	0.0332	0
Tumor	0.0214	0.075	0.025	13	3	0.0255	-0.0077
Fibrous	0.0214	0.060	0.010	11	1	0.0302	-0.0030

Result of reconstruction

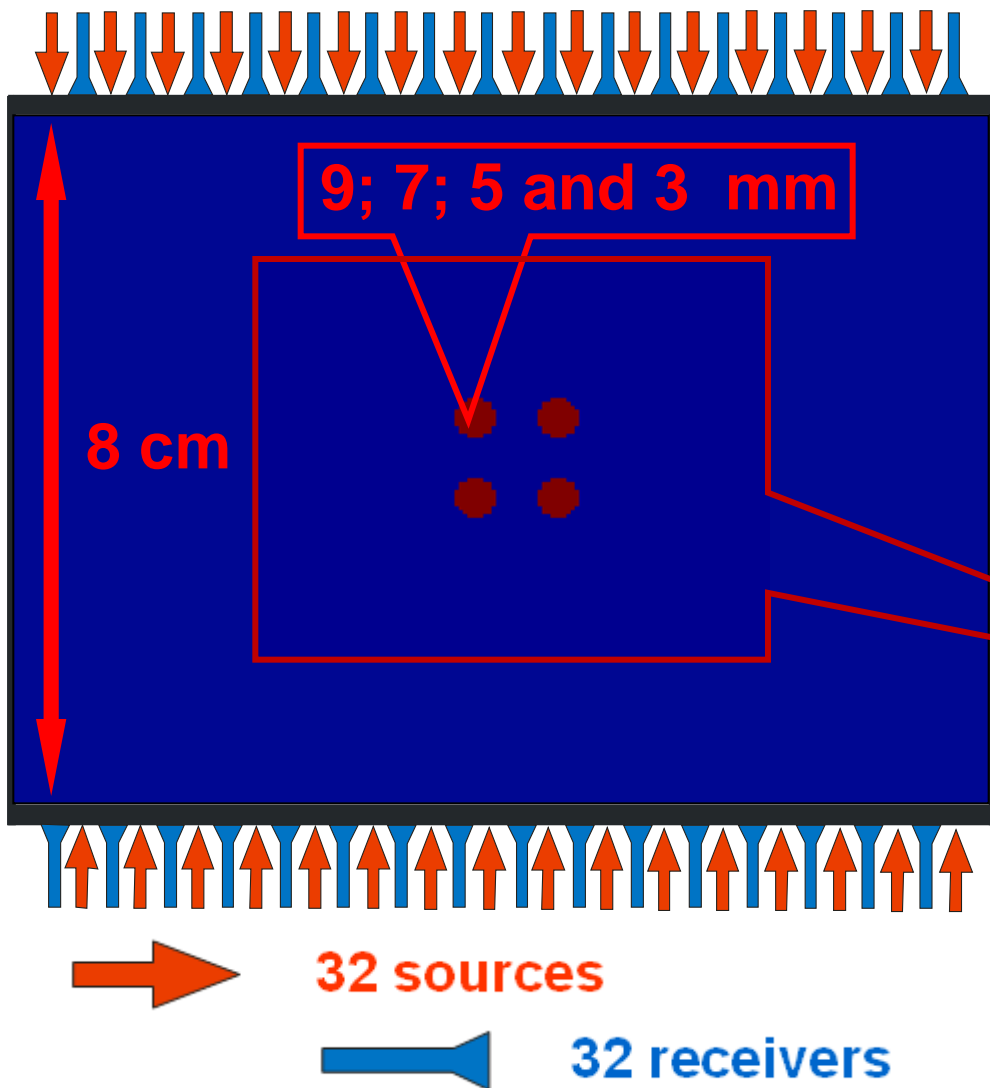
disturbance of
absorption coefficient





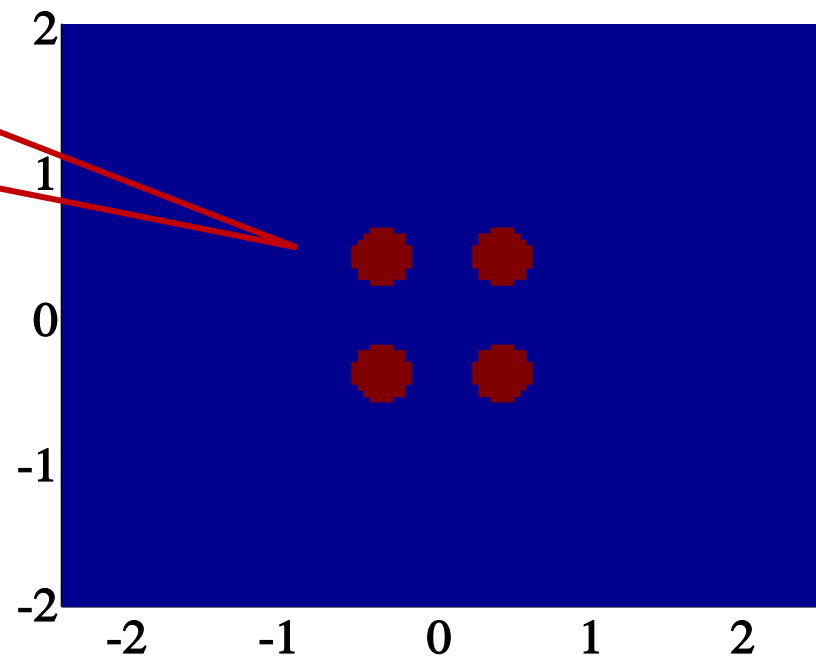
disturbance of
diffusion coefficient



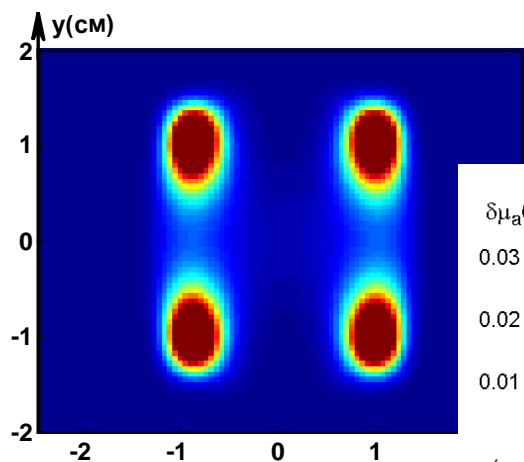
The phantoms for evaluating resolution



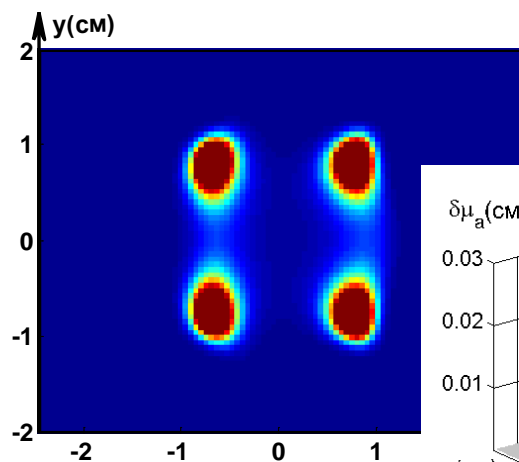
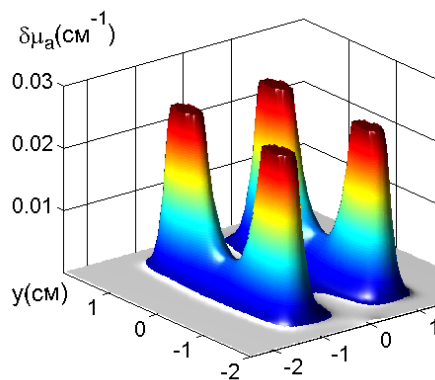
-  $\mu_a = 0.05 \text{ cm}^{-1}$
 $D = 0.0332 \text{ cm}$
-  $\mu_a = 0.075 \text{ cm}^{-1}$
 $D = 0.0332 \text{ cm}$



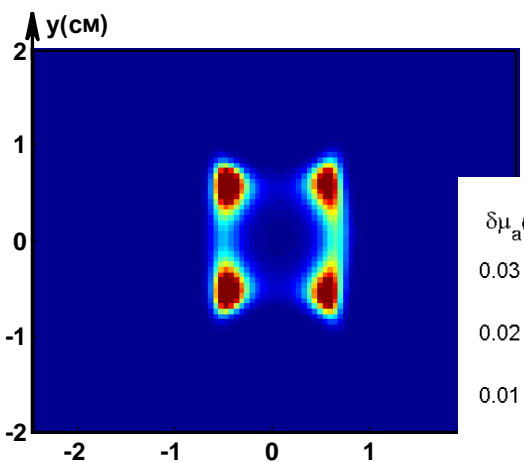
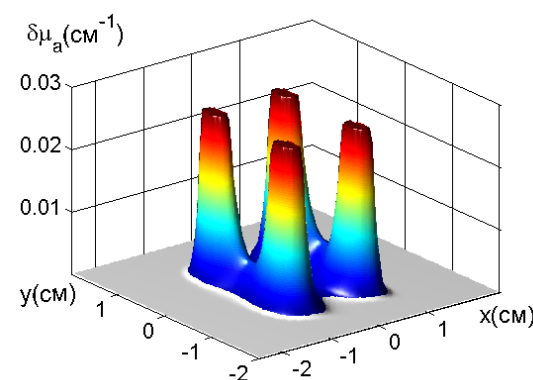
Results of reconstruction



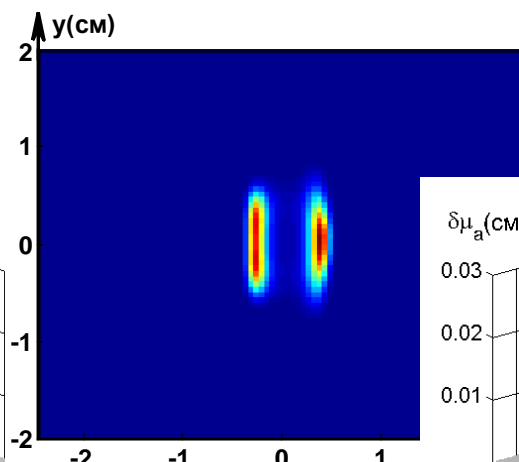
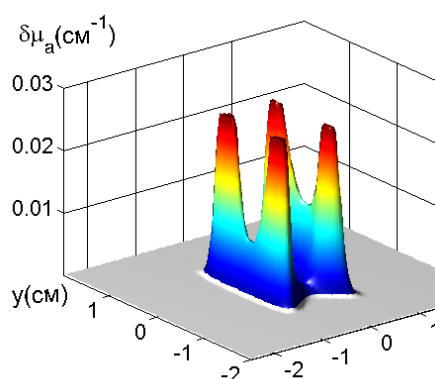
9 mm



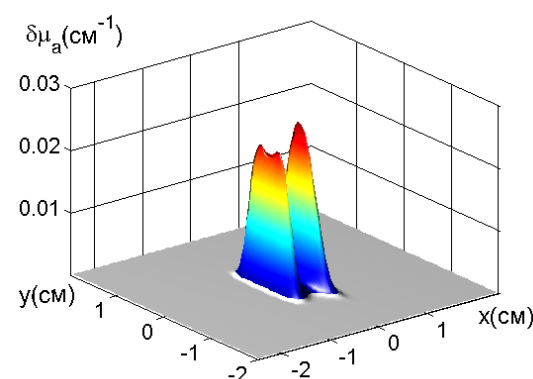
7 mm



5 mm

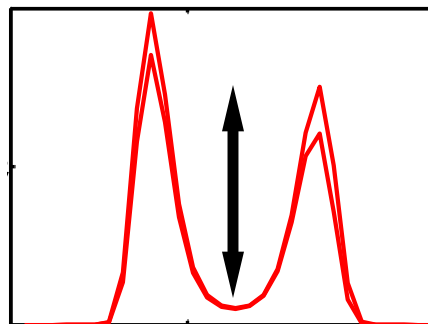
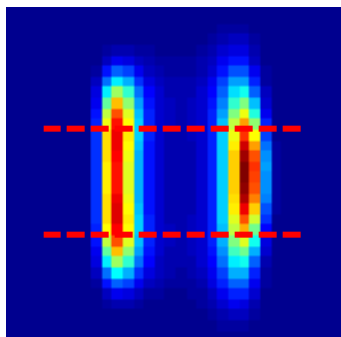


3 mm



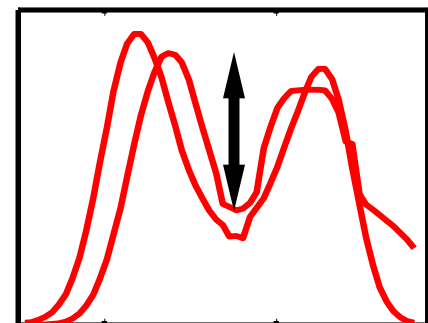
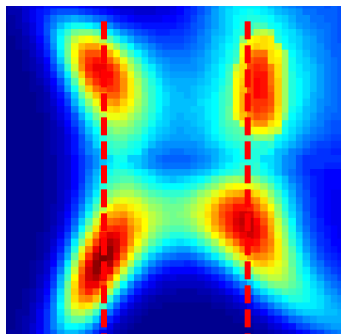
Resolution analysis

- In the centre of an 8-cm-thick object, the transverse resolution is better than 3 mm.

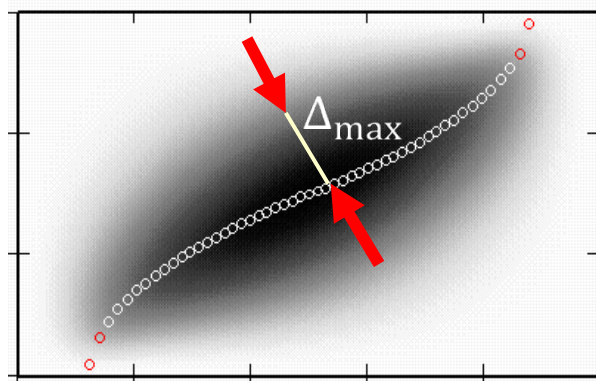


Modulation is more than **60%**

- The longitudinal resolution is slightly worse than the transverse one. It is close to 4 mm.



Modulation is more than **40%**



➤ The photon average trajectory (PAT)

$$\mathbf{R}(\mathbf{r}_s, t_s, \mathbf{r}_d, t) = \int_{\mathbf{v}} \mathbf{r} \frac{G(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} d^3 r$$

➤ The root-mean-square deviation of photons from the PAT

$$\Delta(\mathbf{r}_s, t_s, \mathbf{r}_d, t) = \left[\int_{\mathbf{v}} |\mathbf{r} - \mathbf{R}(\mathbf{r}_s, t_s, \mathbf{r}_d, t)|^2 \frac{G(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} d^3 r \right]^{1/2}$$

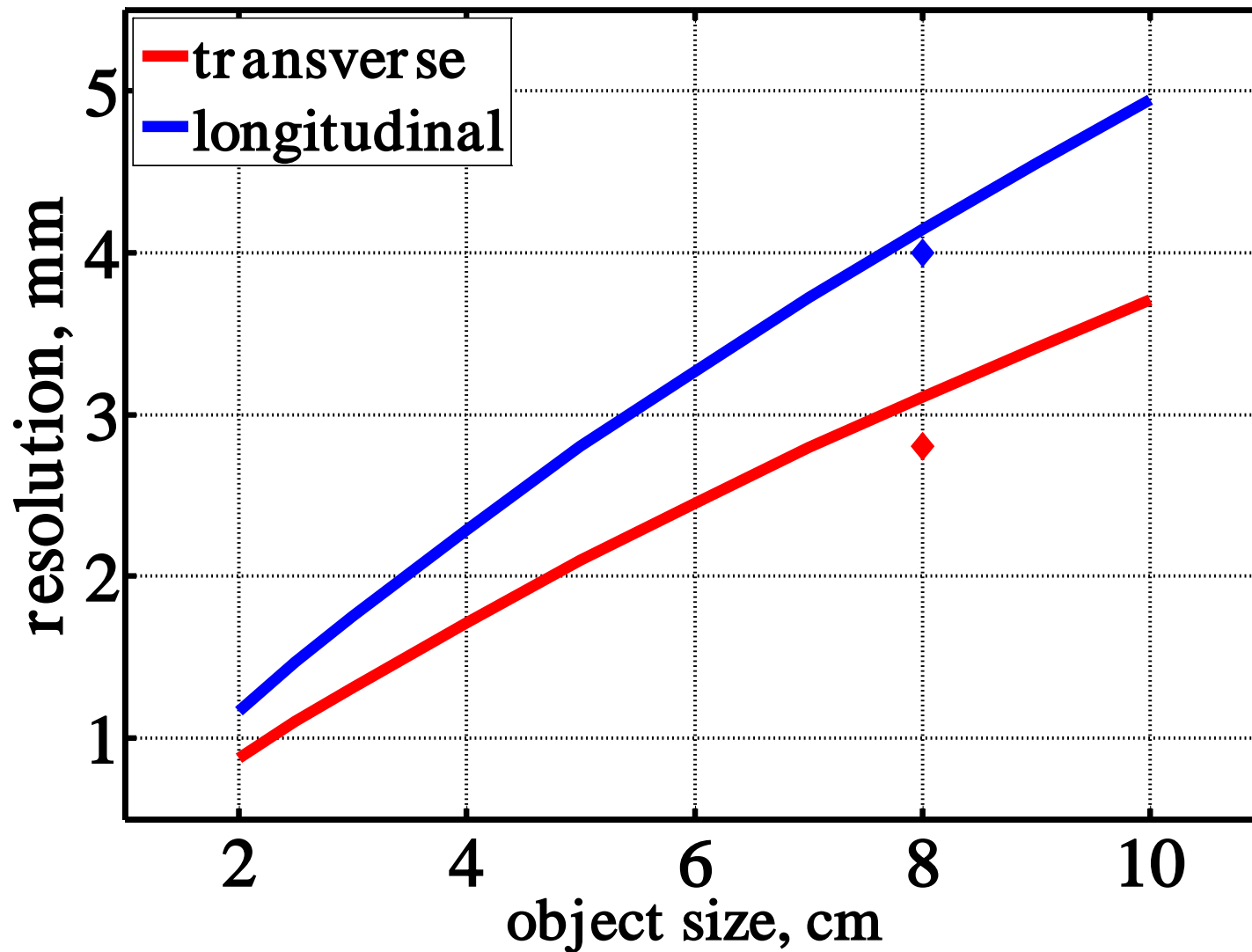
➤ The resolution limit

$$\delta_{\text{lim}} \cong \xi \cdot \Delta_{\text{max}}$$

V.V. Lyubimov, *Opt. Spectrosc.* 86: 251 (1999)

A.B. Konovalov, V.V. Vlasov, *Quantum Electron.* 44: 239 (2014)

Theoretical resolution limit



- ❑ For parallel-plate transmission geometry, the weight functions responsible for optical inhomogeneity reconstruction can be evaluated semi-analytically with the equivalent inverse source method.
- ❑ Our implementation of Lyubimov's perturbation model allows a record-breaking spatial resolution to be achieved (better than 3 and 4 mm inside an 8-cm-size object in transverse and longitudinal directions, respectively).

Publications we refer to

- V.V. Lyubimov, **Optical tomography of highly scattering media by using the first transmitted photons of ultrashort pulses**, *Opt. Spectrosc.* 80(4): 616-619 (1996)
- V.V. Lyubimov, **On the spatial resolution of optical tomography of strongly scattering media with the use of the directly passing photons**, *Opt. Spectrosc.* 86(2): 251-252 (1999)
- A.B. Konovalov, V.V. Vlasov, A.G. Kalintsev, O.V. Kravtsenyuk, and V.V. Lyubimov, **Time-domain diffuse optical tomography using the analytic statistical characteristics of photon trajectories**, *Quantum Electron.* 36(11): 1048-1055 (2006)
- A.B. Konovalov , V.V. Vlasov, A.S. Uglov, and V.V. Lyubimov, **A semi-analytical perturbation model for diffusion tomogram reconstruction from time-resolved optical projections**, *Proc. SPIE* 8088: 80880T (2011)
- A.B. Konovalov, V.V. Vlasov, and V.V. Lyubimov, **Statistical characteristics of photon distributions in a semi-infinite turbid medium: Analytical expressions and their application to optical tomography**, *Optik* 124(23): 6000-6008 (2013)
- A.B. Konovalov and V.V. Vlasov, **Theoretical limit of spatial resolution in diffuse optical tomography using a perturbation model**, *Quantum Electron.* 44(3): 239-246 (2014)
- A.B. Konovalov and V.V. Vlasov, **Calculation of the weighting functions for the reconstruction of absorbing inhomogeneities in tissue by time-resolved optical projections**, *Quantum Electron.* 44(8): 719-726 (2014)
- A.B. Konovalov and V.V. Vlasov, **Total variation based reconstruction of scattering inhomogeneities in tissue from time-resolved optical projections**, *Proc. SPIE* 9917: 99170S (2016)

The authors thank you for your time!



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