



Russian Federal Nuclear Center –
Zababakhin Institute of Applied Physics



“ROSATOM” STATE CORPORATION

Early photon fluorescence molecular tomography with Lyubimov reconstruction model: sensitivity functions and resolution estimates

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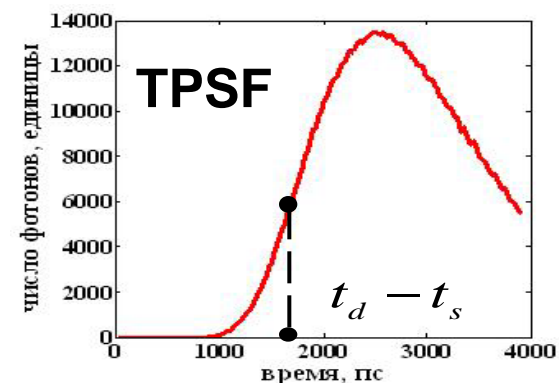
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- 1. Lyubimov reconstruction model: basic formulas**
- 2. Sensitivity functions: comparison with diffusion tomography**
- 3. Lyubimov criterion for resolution estimation: some results for transmission imaging**
- 4. Resolution estimates for reflectance fluorescence tomography**
- 5. Conclusion and future research**

Time-resolved optical projections (DOT)

$$g(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = \frac{\Gamma_0(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d} - \Gamma(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}{\Gamma_0(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}$$

$\Gamma(\mathbf{r}_s, t_s, \mathbf{r}_d, t)$ is the temporal point spread function (TPSF)



Ratio of fluorescence flux to exciting radiation flux (FMT)

$$g_f(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = \frac{\Gamma_f(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}{\Gamma_e(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}$$

Here e, f are indices with respect to exciting radiation and fluorescence, respectively

□ System of diffusion equations

$$\frac{1}{c} \frac{\partial}{\partial t} \varphi_e(\mathbf{r}, t) - D_e \Delta \varphi_e(\mathbf{r}, t) + \mu_{ae}(\mathbf{r}) \varphi_e(\mathbf{r}, t) = S(\mathbf{r}, t)$$

$$\frac{1}{c} \frac{\partial}{\partial t} \varphi_f(\mathbf{r}, t) - D_f \Delta \varphi_f(\mathbf{r}, t) + \mu_{af}(\mathbf{r}) \varphi_f(\mathbf{r}, t) = S_f(\mathbf{r}, t)$$

$$S_f(\mathbf{r}, t) = \gamma \int_{t_s}^t \frac{\delta \mu_{af}(\mathbf{r})}{\tau_n} \varphi_e(\mathbf{r}, t') \exp\left(-\frac{t-t'}{t_n}\right) dt'$$

□ Asymptotic estimate for the source function

$$S_f(\mathbf{r}, t) = \frac{\gamma \delta \mu_{af}(\mathbf{r}) \cdot 4D_e c t^2}{\tau_n |\mathbf{r}|^2 + 4D_e c t^2} \varphi_e(\mathbf{r}, t)$$

Solutions for the photon densities

$$\varphi_f(\mathbf{r}, t) = \int_{t_s}^t c dt' \int_V \frac{\gamma \delta \mu_{af}(\mathbf{r}') \cdot 4D_e c t'^2}{\tau_n |\mathbf{r}'|^2 + 4D_e c t'^2} \varphi_e(\mathbf{r}', t') G_f(\mathbf{r} - \mathbf{r}', t - t') d^3 r'$$

$$\varphi(\mathbf{r}, t) = \int_V G(\mathbf{r} - \mathbf{r}', t - t') \varphi(\mathbf{r}', t) d^3 r'$$

$$\frac{\varphi_f(\mathbf{r}, t)}{\varphi_e(\mathbf{r}, t)} = \int_{t_s}^t c dt' \int_V \frac{\gamma \delta \mu_{af}(\mathbf{r}') \cdot 4D_e c t'^2}{\tau_n |\mathbf{r}'|^2 + 4D_e c t'^2} \frac{C_f(\mathbf{r} - \mathbf{r}', t - t')}{G_e(\mathbf{r} - \mathbf{r}', t - t')} \\ \times \frac{\varphi_e(\mathbf{r}', t') G_e(\mathbf{r} - \mathbf{r}', t - t')}{\int_V \varphi_e(\mathbf{r}', t') G_e(\mathbf{r} - \mathbf{r}', t - t') d^3 r'} d^3 r'$$

Equation for the flux ratio

$$\frac{\Gamma_f(\mathbf{r}_s, t_s, \mathbf{r}_d, t) |_{t=t_d}}{\Gamma_e(\mathbf{r}_s, t_s, \mathbf{r}_d, t) |_{t=t_d}} = \gamma \int_{t_s}^{t_d} c dt \int_V \frac{\delta\mu_{af}(\mathbf{r}) \cdot 4D_e c t^2}{\tau_n |\mathbf{r}|^2 + 4D_e c t^2} \times \frac{\frac{\partial}{\partial \eta} G_f(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial \eta} G_e(\mathbf{r}_d - \mathbf{r}, t_d - t)} \times \frac{\varphi_e(\mathbf{r}, t) \frac{\partial}{\partial \eta} G_e(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\int_V \varphi_e(\mathbf{r}, t) \frac{\partial}{\partial \eta} G_e(\mathbf{r}_d - \mathbf{r}, t_d - t) d^3 r} d^3 r$$

$\partial/\partial\eta$ is the derivative in direction of the outer normal to the boundary at the point \mathbf{r}_d



Our simplifying assumptions

- The scattering medium and the fluorescence inhomogeneity have identical optical parameters $\mu_{ae} \cong \mu_{af}$ and $D_e \cong D_f$.
- The Green function derivatives of exciting radiation and fluorescence are equal each other.
- The velocity of the center of instantaneous photon distributions is constant in the most part of the volume.

Resulting equation that describes the model

$$\frac{\Gamma_f(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}}{\Gamma_e(\mathbf{r}_s, t_s, \mathbf{r}_d, t) \Big|_{t=t_d}} \cong \int_V W_{\delta\mu_{af}}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d, \mathbf{r}) \delta\mu_{af}(\mathbf{r}) d^3r, \quad \text{where}$$

$$W_{\delta\mu_{af}}(\mathbf{r}_s, t_s, \mathbf{r}_d, t_d) = \int_{t_s}^{t_d} \frac{4\gamma D_e c^2 t^2}{\tau_n |\mathbf{r}|^2 + 4D_e c t^2} \times \frac{G_e(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial \eta} G_e(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial \eta} G_e(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} dt$$

is the sensitivity function that is responsible for reconstruction of the fluorophore absorption coefficient

Diffuse optical tomography of absorbing inhomogeneities

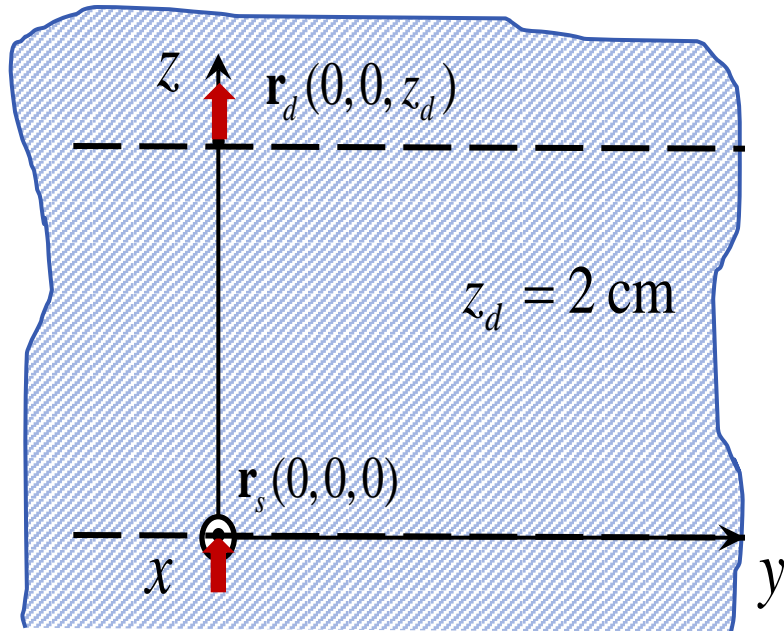
$$W_{\mu_a}(\mathbf{r}_s, \mathbf{r}_d, \mathbf{r}, t_d) = c \int_0^{t_d} \frac{G(\mathbf{r} - \mathbf{r}_s, t) \partial G(\mathbf{r}_d - \mathbf{r}, t_d - t) / \partial \eta}{\partial G(\mathbf{r}_d - \mathbf{r}_s, t_d) / \partial \eta} dt$$

A.B. Konovalov, V.V. Vlasov, *Quantum Electron.* 44: 719 (2014)

Fluorescence molecular tomography

$$W_{\delta\mu_{af}}(\mathbf{r}_s, \mathbf{r}_d, \mathbf{r}, t_d) = c\gamma \int_0^{t_d} \frac{4Dct^2}{\tau_n |\mathbf{r}|^2 + 4Dct^2} \frac{G(\mathbf{r} - \mathbf{r}_s, t) \partial G(\mathbf{r}_d - \mathbf{r}, t_d - t) / \partial \eta}{\partial G(\mathbf{r}_d - \mathbf{r}_s, t_d) / \partial \eta} dt$$

Transmission geometry as a simplest example



$$G_e(\mathbf{r}', \mathbf{r}, t', t) =$$

$$= \left[4\pi Dc(t-t') \right]^{-3/2} \exp \left[-\mu_a c(t-t') - \frac{(x-x')^2 + (y-y')^2 + (z-z')^2}{4Dc(t-t')} \right]$$

$$\frac{G(\dots) \partial G(\dots) / \partial \eta}{\partial G(\dots) / \partial \eta} = \frac{z_d - z}{z_d} (4\pi Dct)^{-3/2} \left(\frac{t_d}{t_d - t} \right)^{5/2} \exp \left[-\frac{x^2 t_d^2 + y^2 t_d^2 + (zt_d - z_d t)^2}{4Dc(t_d - t) t t_d} \right]$$

The banana-shaped distributions

$$\mu_a = 0.05 \text{ мм}^{-1}$$

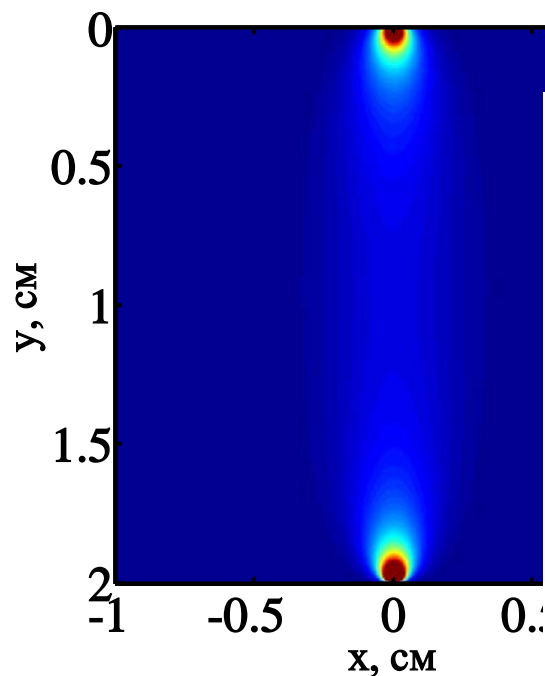
$$\mu'_s = 1.6 \text{ мм}^{-1}$$

$$t_d = 200 \text{ нс}$$

$$c = 0.214 \text{ мм/нс}$$

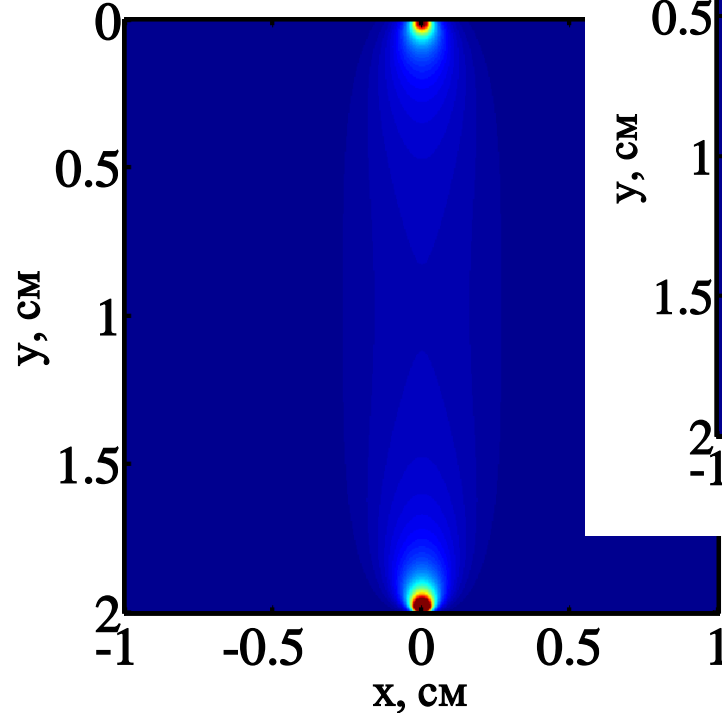
$$D = 0.19 \text{ мм}$$

FMT

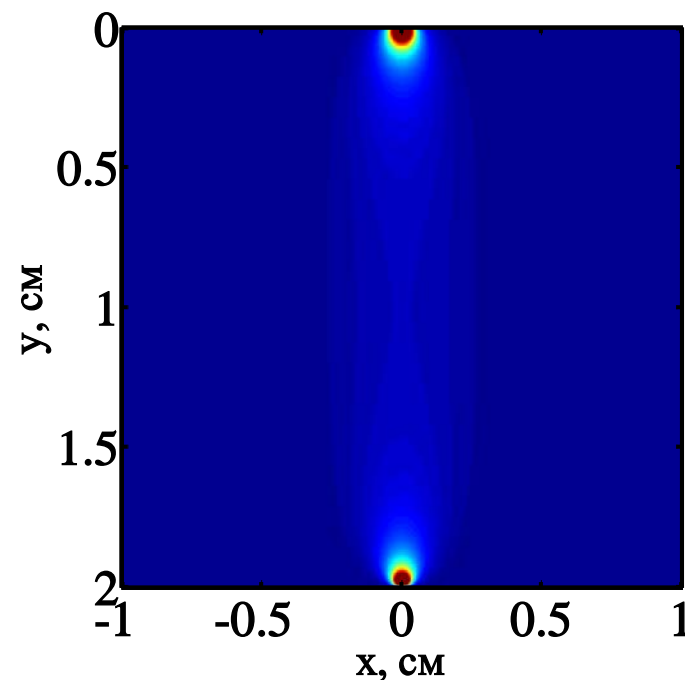


$$\tau_n = 1000 \text{ нс}$$

DOT



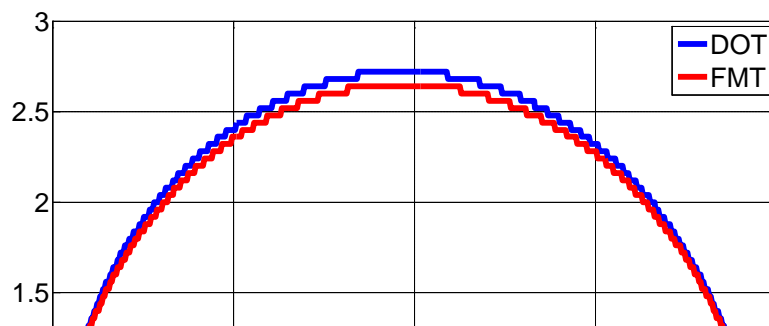
FMT



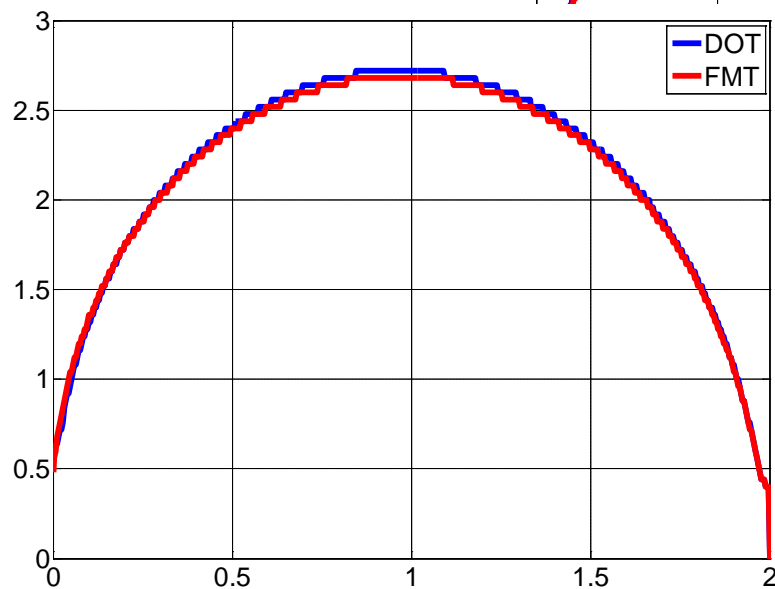
$$\tau_n = 4000 \text{ нс}$$

Standard deviation plots

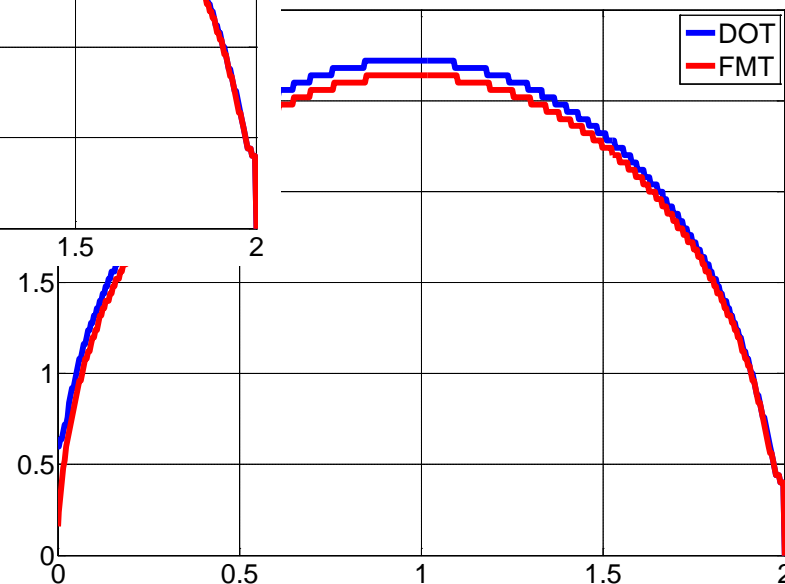
$\tau_n = 1000 \text{ пс}$

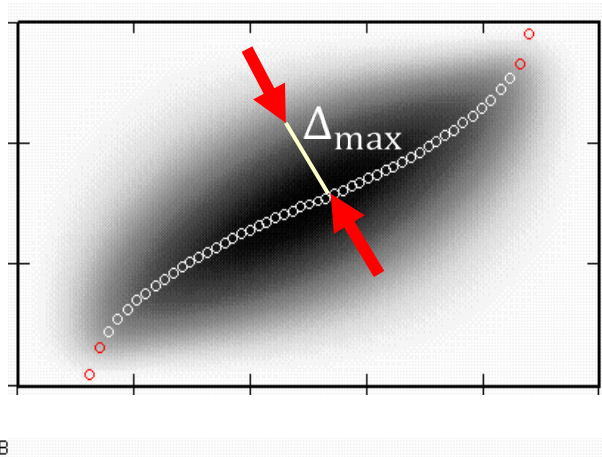


$\tau_n = 50 \text{ пс}$



$\tau_n = 4000 \text{ пс}$





➤ The photon average trajectory (PAT)

$$\mathbf{R}(\mathbf{r}_s, t_s, \mathbf{r}_d, t) = \int_V \mathbf{r} \frac{G(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} d^3 r$$

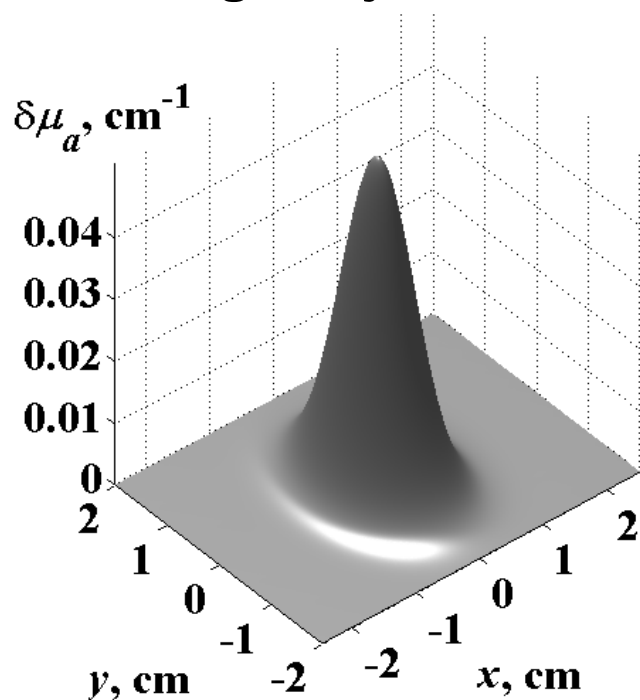
➤ The root-mean-square deviation of photons from the PAT

$$\Delta(\mathbf{r}_s, t_s, \mathbf{r}_d, t) = \left[\int_V |\mathbf{r} - \mathbf{R}(\mathbf{r}_s, t_s, \mathbf{r}_d, t)|^2 \frac{G(\mathbf{r} - \mathbf{r}_s, t - t_s) \frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}, t_d - t)}{\frac{\partial}{\partial \eta} G(\mathbf{r}_d - \mathbf{r}_s, t_d - t_s)} d^3 r \right]^{1/2}$$

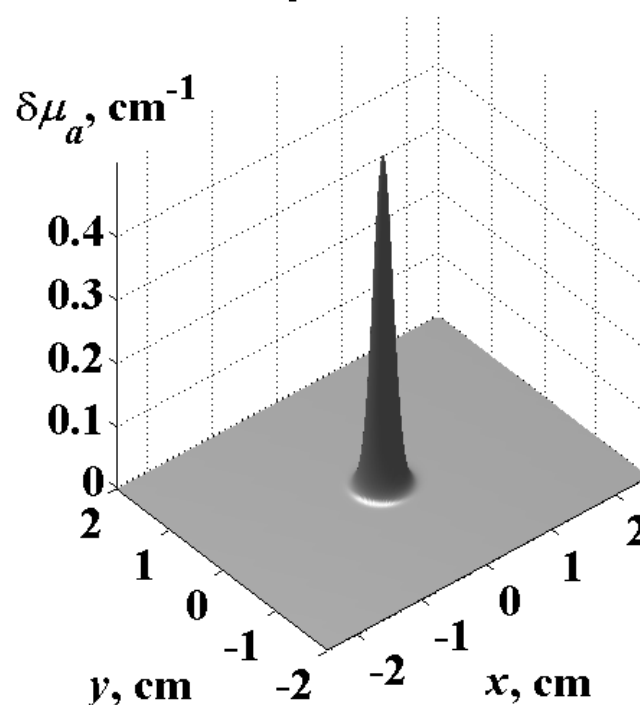
V.V. Lyubimov, *Opt. Spectrosc.* 86: 251 (1999)

V.V. Lyubimov et al., *Phys. Med. Biol.* 47: 2109 (2002)

Average trajectories



Banana-shaped distributions

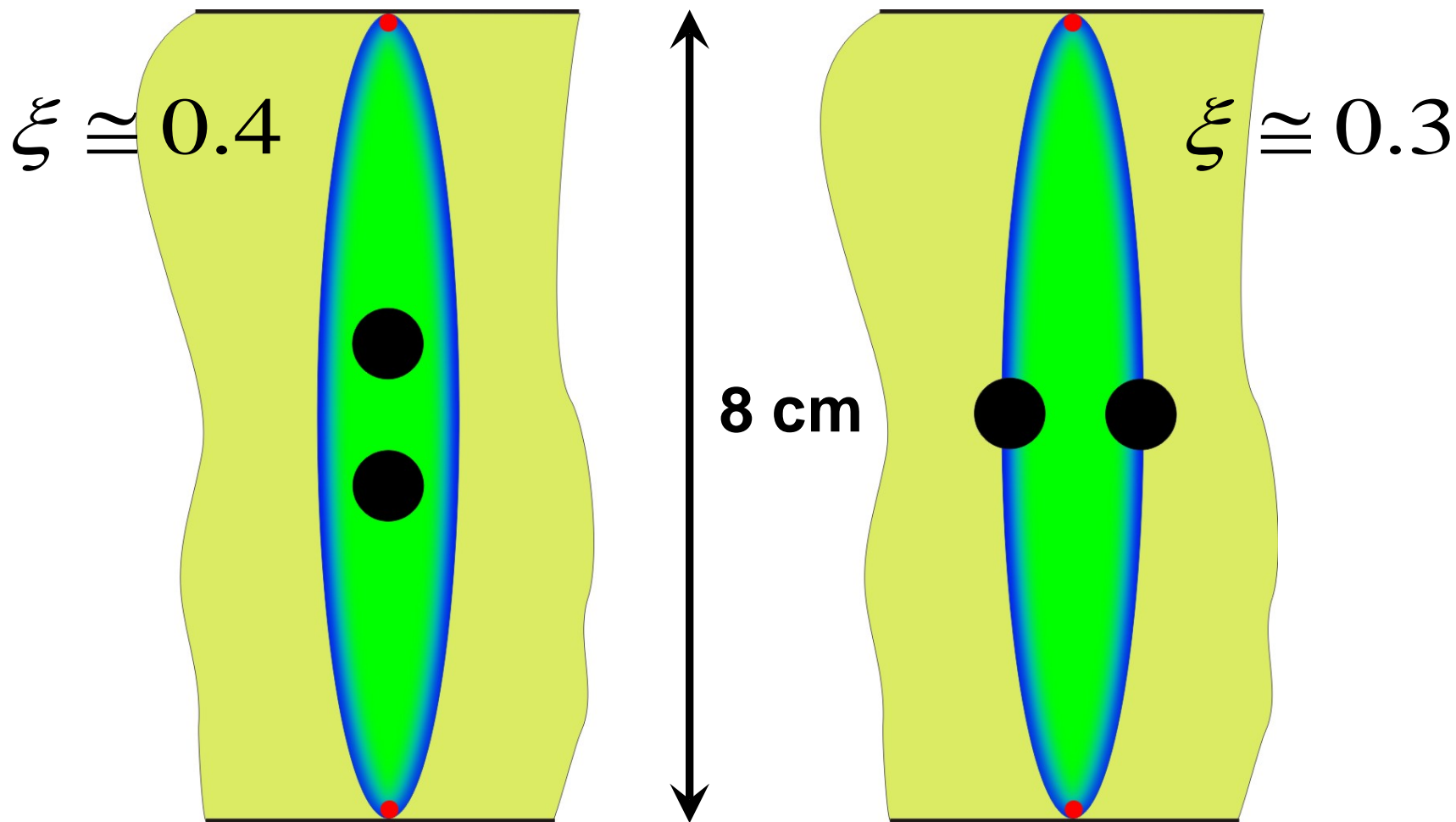


$$\delta_{\text{lim}} \cong \xi \cdot \Delta_{\text{max}},$$

where ξ is a coefficient that depends on the geometry and the reconstruction technique

A.B. Konovalov, V.V. Vlasov, *Quantum Electron.* 44: 239 (2014)

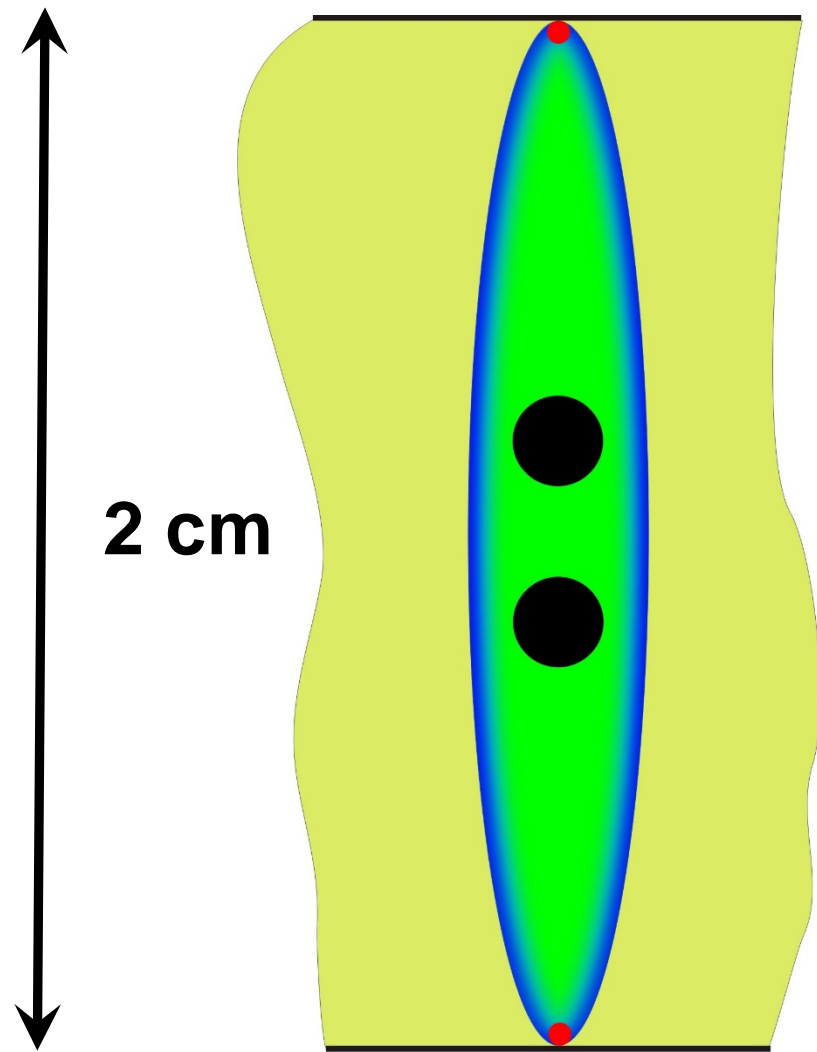
Some estimates for coefficient ξ



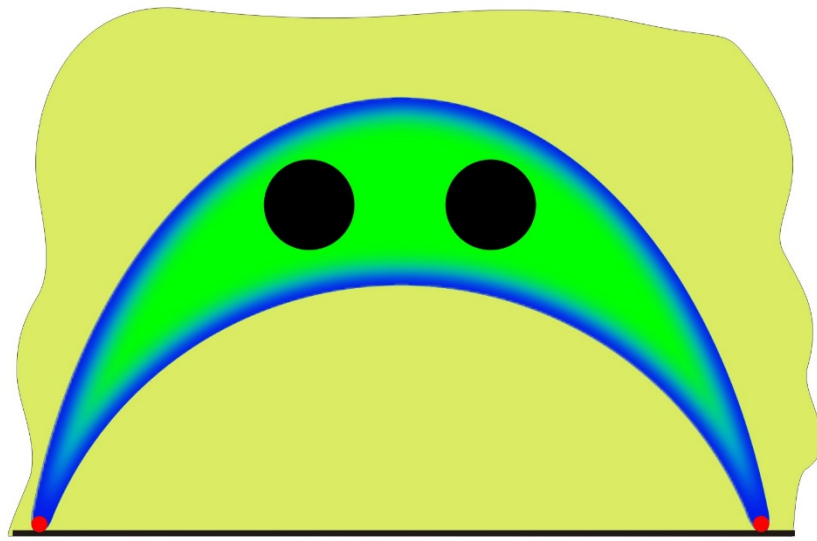
A.B. Konovalov, V.V. Vlasov, Quantum Electron. 44: 719 (2014)



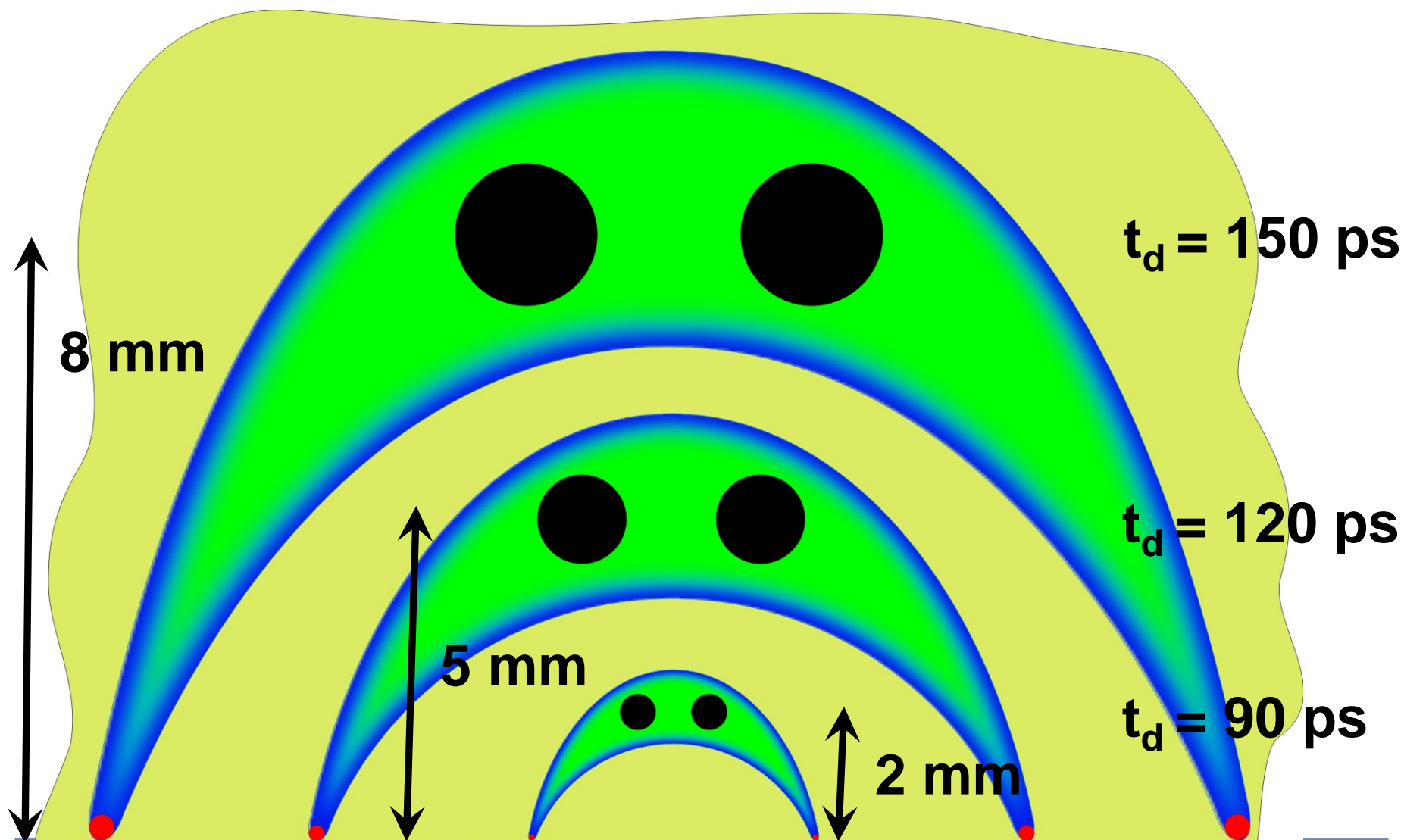
Comparison of two geometries



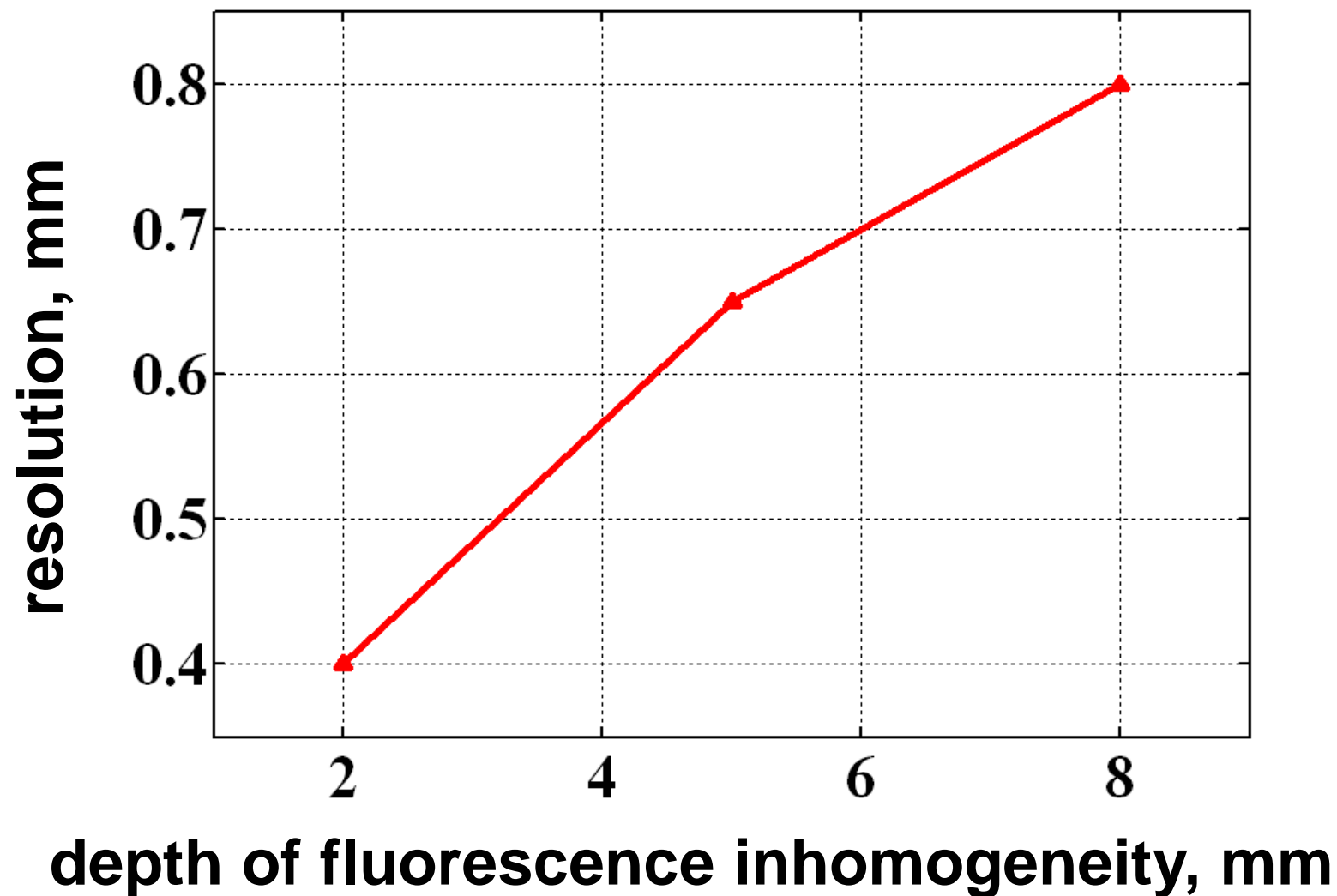
$$\xi \cong 0.4$$



Banana-shaped zones for different depths



Resolution for reflectance FMT





- **According to our theoretical estimates Lyubimov model can reconstruct fluorescence tomograms with high – submillimeter – resolution .**
- **Our further research is aimed at developing a numerical experiment to verify the theoretical results .**

Publications we refer to

- V.V. Lyubimov, **Principles of fluorescence laser tomography of strongly scattering media**, *Opt. Spectrosc.* 88(2): 282-285 (2000)
- A.B. Konovalov and V.V. Vlasov, **Calculation of the weighting functions for the reconstruction of absorbing inhomogeneities in tissue by time-resolved optical projections**, *Quantum Electron.* 44(8): 719-726 (2014)
- V.V. Lyubimov, **On the spatial resolution of optical tomography of strongly scattering media with the use of the directly passing photons**, *Opt. Spectrosc.* 86(2): 251-252 (1999)
- V.V. Lyubimov, A.G. Kalintsev, A.B. Konovalov et al. **Application of the photon average trajectories method to real-time reconstruction of tissue inhomogeneities in diffuse optical tomography of strongly scattering media**, *Phys. Med. Biol.* 47(12): 2109-2128 (2002)
- A.B. Konovalov and V.V. Vlasov, **Theoretical limit of spatial resolution in diffuse optical tomography using a perturbation model**, *Quantum Electron.* 44(3): 239-246 (2014)

The authors thank you for your time!



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